Use of preoperative assessment of positionally induced cyclotorsion: a video-ocularographic study

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Purpose: Positionally induced cyclotorsion could be an important factor concerning correction of astigmatism in refractive surgery. The method of binocular three dimensional infrared video-ocularography (3D-VOG) was used to determine a possible influence of body position on cyclotorsion.

Methods: 38 eyes (19 healthy subjects, median value of age 25.5) with normal binocular vision were examined using 3D-VOG. This method records ocular motions and positions of both eyes simultaneously in the x, y, and z axis. Cycloposition of the eyes was recorded first in a seated position (both eyes open, test 1), then in a supine position (right eye closed, test 2), occlusion of both eyes (test 3), both eyes open (test 4). Cyclovergence was calculated as the difference between the right and the left eye positions.

Results: The range of cyclotorsion of the right and left eye in all four tests was between 1.13˚ excycloversion and 0.34˚ incycloversion. There was no statistically significant difference of the median values for torsion for the four test situations. Concerning the influence of body position on cyclotorsion, a statistically significant difference between the different test positions and settings did not exist. Median values for right/left torsion/cyclovergence were: 0.17/0.04/0.02 (test 1), −0.31/−0.71/−0.16 (test 2), −1.09/−0.60/0.82 (test 3), 0.28/0.28/−0.82 (test 4).

Conclusions: Cyclotorsion does not significantly change between seated and supine position in subjects with normal binocular vision and stable fixation. In these subjects, an erroneous refractive surgery due to incorrect measurement of the axis of astigmatism in the seated position and performing the refractive surgery in the supine position, is very unlikely.

Methods

Subjects

Thirty eight eyes from 19 subjects with no known abnormalities of their visual system and stereopsis of at least 40 seconds of arc were included in the study. Median value of age was 25.5 years. The subjects had a refractive error of 0.08 D (median value) of the mean spherical equivalent and standard deviation of 0.08. All subjects were positioned comfortably, first in a seated upright and then in a supine position. Strabismus (especially dissociated vertical divergence, DVD) and any organic eye disease were excluded by thorough ophthalmological examination including biomicroscopy, indirect ophthalmoscopy, refractometry or retinoscopy in cycloplegia, cover test, assessment of ocular motility, prism and cover test, verification of stable, central fixation by using the so called “Haidinger Büschel” and afterimage, determination of stereopsis by the Lang stereotest and the Titmus test. All subjects had normal visual acuity in both eyes and random dot stereopsis of at least 40 seconds of arc. The study followed the Declaration of Helsinki. The nature of the study had been clearly explained and informed consent was obtained from all subjects before testing.

Abbreviations: 3D-VOG, three dimensional video-ocularography; DVD, dissociated vertical divergence; LT, left torsion; RT, right torsion
Binocular infrared three dimensional video-ocularography

For recording eye positions, the method of three dimensional infrared video-ocularography (3D-VOG) was used. The patient had to put on a mask, which is similar to a diving mask, as shown in figure 1. In order to obtain a stable position, a chin rest together with a bite bar was used.

The device is formed of two high resolution video cameras and 3 infrared LED sources in a pair of goggles and a computer with especially designed video cards. The system is commercially available (Senso Motoric Instruments GmbH, Teltow, Germany). The position of the eyes is analysed in three dimensions. This is performed for the calculation of horizontal and vertical position movements and deviations by the “black pupil technique”—that is, by infrared measurement and localisation of the individually calibrated pupil. The difference in horizontal and vertical position between both eyes gives the angle of deviation, and the graph of these positions, measured all 0.02 seconds, leads to the horizontal and vertical eye movements. We will use the term cycloposition for expression cyclotorsion. Both describe the actual static deviation of the sole right or sole left eye in the sagittal or torsional axis from the null position. The term cycloduction describes a dynamic deviation or movement in this axis. Thus, connecting the large amount of data for cycloposition will give a graph showing the cycloduction or cyclodutional movement. It is important to recognise that all measurements for cycloposition reflect a relative measurement, which starts from 0 at an arbitrary point (time zero seconds) and position (0° cycloposition). The cyclovergence was calculated as the difference between the right and the left eye positions in the torsional axis—that is, the y axis of Fick’s coordinate system (RE-LE).

The determination of the cycloposition and cycloduction of each eye (the y axis in Fick’s coordinate system), is enabled by measuring a selected iris segment and its deviations (fig 2). Iris structures are overlayed and compared in order to determine the amount of rotation around the visual axis. Illumination of each eye was provided by three infrared LED sources with a wavelength of 920 nm (intensity <1 mW/cm²). Torsional movements were sampled with a frequency of 50 Hz. A measurement was taken every 0.02 seconds. Thus, 3000 measurements for both torsion of the right and left eye (cycloposition) could be obtained during a measurement of 1 minute. In studies comparing the accuracy of binocular infrared video-ocularography with other techniques, a more detailed description of the method can be found.

Positive values express incyclotorsion and negative values express excyclotorsion of the eye.

Cycloposition of the eyes was recorded first in a seated position with both eyes open (test 1) then, in order to obtain a quite realistic experimental setting, in a supine position, beginning with the right eye closed (test 2), then with occlusion of both eyes (test 3), followed by a fourth measurement with both eyes open in the supine position (test 4). Occlusion of one or both eyes was achieved with the help of a piece of metal put on the front side of the recording mask serving as an occluder. Each of these four tests was recorded for 1 minute allowing measurement of 3000 positions. A diagonal cross of 3° presented in primary gaze served as a fixation target. Primary gaze is determined clinically and not derived from experimental calculations of Listing’s plane. The fixation distance for the seated and supine position was 4m. The calibration made at the initial position at the starting time (zero seconds) should give the positional values 0;0;0. According to the aim of our study and the negligible horizontal and vertical deviations, the key measurement was that of the cycloposition.

Data collection was performed with the software that accompanies the system. The ocular cyclotorsion was assessed by calculation of the angular displacement of the position of a defined iris segment (fig 2). Therefore, grey levels of a specific iris segment serving as a reference profile were extracted and a correlation of the profile with the neighboring segments was performed for each video frame. The software that accompanies the system allows the calculation of the so called quality factor Q (between 0.0 and 1.0) representing the concordance between the reference profile and that of the same iris segment of each consecutive frame during recording. The instruction manual suggests a quality factor of 0.3 or better in order to reduce the risk of false data. In our examinations, the quality factor was higher than 0.8.

Statistical analyses

The statistical calculations for comparison of ocular cyclotorsion of both eyes were performed using the Wilcoxon matched pairs signed rank test. In order to work out the relationship between body position and induced in- or excyclotorsion concerning the different test situations (test 1–4), we used a multivariate analysis of variance ($p = 0.05$). Median values and 95% confidence intervals for right torsion (RT), left torsion (LT), and cyclovergence for the four tests were calculated.
The measured cyclotorsional deviations were actually very small. In the seated (test 1) as well as in the supine position with both eyes opened (tests 1 and 4), the cycloposition of both eyes was located around 0.11° of incycloposition. This “test position” shifts in the supine position with occlusion of either one (test 2) or both eyes (test 3) to a cycloposition penduling around 1°–2° of encycloposition. These oscillations of both eyes were not conjugated—that is, they were in some of the small time intervals clockwise, in other time intervals anticlockwise. The shift was detectable in the cycloposition of the right and left eye equally in all patients. In the supine position with opening of both eyes, cyclotorsion showed fewer artifacts compared with the supine position with both eyes closed, but was still differing more from zero than in the seated position, although statistically not significantly. In a supine position with occlusion of one eye, cyclotorsion of both eyes was higher, but not statistically significant, than in the seated position. When both eyes were closed in the supine position, cyclotorsion was less regular with a bigger difference from zero compared with the seated and supine position with occlusion of only one eye (see table 1).

Statistical analysis of the different test positions did not show any positionally induced cyclotorsion—that is, we did not find a statistically significant difference of the eyes’ cyclotorsion between seated and supine position either with or without occlusion of one or both eyes. There also were no statistically significant differences between right and left eyes for the seated and supine test positions.

Figures 3 to 8 show examples of the cyclotorsion of the right/left eye for one of the normal subjects for the four test conditions. All subjects showed similar changes of in- and excycloposition for the different test positions and settings. The vertical peaks—for example, in figure 4 peaks exceeding 1 degree of excycloposition—are artifacts caused by blinking. This could be proved by monitoring and observation of the patient’s lids and eyes during the measurement. Figure 3 shows the cyclotorsion of the right eye for one subject with both eyes open in a seated position (test 1). Positive values express incycloposition and negative values express excycloposition of the eye. Figure 4 shows the first 3 seconds of the cyclotorsion of both eyes (blue line: right eye; green line: left eye) for the same subject referred to in figure 3 for test 1. The range of cycloposition of the right (left) eye is between 1.2° (1.8°) incycloposition and 0.6° (2.0°) excycloposition. When both eyes were open in the supine position (test 4), we found an oscillation of the eye position between an encycloposition of 1.4° and and incycloposition of 2.4° (fig 5). Figure 6 again shows the first 3 seconds for this test situation. While the range of cyclotorsion for the right eye was higher than for the left eye, a statistically significant difference did not exist. Figure 7 expresses cyclotorsion of the right eye for the same subject referred to in figures 3–6 with the right eye closed in a supine position (test 2) and in figure 8, cyclotorsion of the right eye for the same subject with occlusion of both eyes in the supine position (test 3), achieved with the help of a piece of metal put on the front side of the recording mask, is shown. In this test situation, cyclotorsion is with a bigger difference from zero compared with the seated and supine position with occlusion of only one eye.

In all examinations, a quality factor higher than 0.8 could be achieved representing data with a high quality level with a minimum of false positive or false negative values. Examinations took 4 minutes in total for each subject. For

**Table 1** Median values (95% confidence interval) for 38 eyes from 19 subjects for right torsion (RT), left torsion (LT), and cyclovergence for the four tests (degree) for a measurement of one minute.

<table>
<thead>
<tr>
<th>Measurement</th>
<th>Test 1</th>
<th>Test 2</th>
<th>Test 3</th>
<th>Test 4</th>
</tr>
</thead>
<tbody>
<tr>
<td>RT</td>
<td>0.17 (-0.06 to 0.4)</td>
<td>-0.31 (-2.42 to 1.8)</td>
<td>-1.09 (-2.47 to 0.29)</td>
<td>0.28 (-0.73 to 1.29)</td>
</tr>
<tr>
<td>LT</td>
<td>0.04 (-0.3 to 0.38)</td>
<td>-0.71 (-1.96 to 0.54)</td>
<td>-0.60 (-3.3 to 2.1)</td>
<td>-1.28 to 1.84</td>
</tr>
<tr>
<td>Cyclovergence</td>
<td>0.02 (-0.41 to 0.45)</td>
<td>-0.16 (-1.2 to 0.88)</td>
<td>0.82 (-0.54 to 2.18)</td>
<td>-0.82 (-3.59 to 1.95)</td>
</tr>
</tbody>
</table>

Test 1: seated position, both eyes open; test 2: supine position, right eye closed; test 3: supine position, both eyes closed; test 4: supine position, both eyes open. Incycloposition is characterised by positive values and excycloposition by negative values.
DISCUSSION

Positionally induced in- or excyclotorsion could be an important factor in the outcome of refractive surgery. Two possible mistakes with clinical significance may occur. Firstly, a simple difference of the axis of astigmatism between the sitting and supine position will lead not only to an erroneous correction of the astigmatism itself, but the whole spherocylindrical correction could be false. This applies especially to the modern flying spot excimer lasers. Secondly, an unpredictable cyclotorsional movement—that is, an oscillation of the y axis of each eye, will result in complex errors of the excimer laser ablation. This would make a tracking system for the torsional movement of the eye absolutely mandatory.

We used the method of binocular three dimensional infrared video-oculography in order to determine a possible influence of body position on cyclotorsion with a very accurate method, and we did not find any statistically significant positionally induced cyclotorsion. Our finding that body position does not have any influence on ocular torsion, is in accordance with previous studies by Tjon-Fo-Sang et al., but as they used different methods, a direct comparison with their results is not possible. Tjon-Fo-Sang found in 13% of a total of 15 persons with normal binocular vision, that statistically significant excyclotorsion occurred when changing from binocular to monocular fixation in a seated position. The same occurred in the supine position in the study of Tjon-Fo-Sang, in which three subjects (20%) showed excyclotorsion when the fixation changed. Therefore Tjon-Fo-Sang et al. found only an influence of the way of fixation—that is, if the patient has binocular fixation with stereopsis, or if the patient has only monocular fixation.

We found that in the seated and supine position with both eyes open, the cycloposition of the right eye and the left eye, respectively, was located approximately around 1° of incyclotorsion. This “rest position” shifts in the supine position with either one or both eyes closed to a cycloposition penduling around 1° to 2° of excyclotorsion. This shift was detectable in the cycloposition of the right and left eye in most patients. In contrast to Gordes et al., all measurements revealed very small deviations from zero in the y axis of the eye in Fick’s coordinate system. As Gordes et al. used the same measurement device, one explanation for their persis-

Figure 5  Cyclotorsion of the right eye for one subject (figs 3 and 4) with both eyes open in a supine position (test 4). The eye position oscillates between an excyclotorsion of 1.4° and an incyclotorsion of 2.4°.

Figure 6  First 3 seconds of the cyclotorsion of both eyes (blue = right eye, green = left eye) for the subject referred to in figures 3–5 for test 4 (that is, both eyes open in a supine position). As in other figures, positive values express incyclotorsion and negative express excyclotorsion of the eye. The range of cyclotorsion of the right eye (1.28° to –0.78°) of this subject is higher than that of the left eye (0.75° to –0.37°) for this time interval, but the difference in ranges is not statistically significant.

Figure 7  Cyclotorsion for the right eye of the subject referred to in figures 3–6 with the right eye closed in a supine position (test 2).
fixating eye. Enright created the word “cyclotorsional noise” as the measured cyclotorsional deviations were very small.

Our experimental setting is quite realistic for a LASIK or LASEK situation, which are currently the most common refractive surgeries. If the patient has normal binocular vision and stable fixation of both eyes, it will in the future neither be necessary to measure corneal topography or ocular aberrations in the supine position in order to avoid uneventful torsional deviations, nor will it be mandatory to implement a device like this 3D-VOG as a tracking device to control torsional deviations. Further investigations will show if our results also apply to subjects without normal binocular vision or unstable fixation. If these subjects show higher cyclotorsions or fluctuations between the sitting and supine position, tracking devices to control the torsion of the eyes will be useful, as described by MacRae et al.12

Figure 8  Cyclotorsion for the right eye for one subject (figs 3–7) with both eyes closed in a supine position (test 3). Cyclotorsion is with a bigger difference from zero compared with the seated and supine position with closure of one eye.

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