Ultrasound enhanced thrombolysis in experimental retinal vein occlusion in the rabbit

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Abstract

Aims—To investigate if it was possible to lower the dose of streptokinase and maintain an effective thrombolysis by adding pulsed low energy ultrasound.

Methods—53 retinal veins in 27 rabbits were occluded by rose bengal enhanced laser treatment. Six rabbits were treated with streptokinase (50 000 IU/kg), 10 rabbits were treated with a low dose of streptokinase (25 000 IU/kg), and 11 rabbits were treated with a low dose of streptokinase (25 000 IU/kg) and pulsed ultrasound during 1 hour. Fluorescein angiography was performed immediately before the thrombolytic treatment and after 12 hours.

Results—In the group treated with streptokinase (50 000 IU/kg) all vessels were open. In the group that was given streptokinase (25 000 IU/kg), 21% of the vessels were open. In the group that was treated with streptokinase (25 000 IU/kg) and ultrasound, 64% of the vessels were open. The difference between groups 2 and 3 is statistically significant (p= 0.011)

Conclusion—Adding pulsed low energy ultrasound makes it possible to lower the dose of streptokinase while maintaining a good thrombolytic effect.

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Retinal vein occlusion is the second most common vascular disease in the human eye. The most severe form of retinal vein occlusion is central retinal vein occlusion (CRVO). There are two forms of CRVO, the ischaemic and the non-ischaemic, both leading to loss of visual acuity. About 20–30% of the CRVOs are ischaemic and the majority of them develop secondary glaucoma and ruberosis. Many different treatments have been tried such as haemodilution, thrombolytic treatment, formation of choriretinal anastomoses, and different drugs that influence the microcirculation. For different reasons, none of these treatments is widely used today, either because of severe side effects or they are considered to be too complicated, such as haemodilution.

Thrombolytic treatment, with streptokinase and tissue plasminogen activator, is one of the most promising methods of treating a thrombus in the eye since it dissolves the clot, allowing the circulation to be re-established within a few hours. The side effects of thrombolytic treatment are haemorrhages and are a great threat. The incidence of severe haemorrhage is around 0.5–1.0%. In a disease such as myocardial infarction, which is life threatening, this incidence of haemorrhage is acceptable, but in a patient with a retinal vein occlusion it is hard to accept life threatening side effects.

Dye enhanced photothrombosis is a method where a dye that absorbs maximally at a specific wavelength is injected intravenously immediately before laser treatment in order to enhance the absorption of the laser light and thus making it possible to use less laser energy. This method easily produces thrombi in the vessels.

Based on earlier in vitro experiences, we wanted to investigate whether it was possible to lower the dose of streptokinase by adding pulsed low energy ultrasound towards a thrombus in the eye. We investigated this in a model of experimental retinal vein occlusion in the rabbit eye.

Methods

Twenty seven albino New Zealand rabbits were used (27 eyes, 53 vessels), each weighing 3–3.5 kg. The rabbits were anaesthetised with a mixture of Ketalar and Rompun. Their pupils were dilated with 1% cyclopentolate eyedrops. The animals were treated according to the guidelines and requirements of the government committee on animal experimentation ethics of the University of Lund and the ARVO convention for animal experimentation ethics.

Occlusion of the retinal veins was performed by dye enhanced photothrombosis. We used the same method to induce thrombi in the retinal veins as has been described previously by Oncel et al. Rose bengal solution, 50 mg/kg (50 mg/ml in sterile water), was injected in an ear vein immediately before the laser treatment. Argon green laser treatments were performed with a power of 0.14 mW, a spot size of 100 µm, and a duration of 0.3 seconds. Each vessel was treated at a distance of a half to one disc diameter from the optic disc, until the blood flow was completely stopped in the vein. About 5–20 laser effects were needed for each vessel.

The rabbits were randomised into three groups—group 1 (six rabbits, six eyes, 12 vessels) was treated with an infusion in an ear vein of 50 000 IU/kg streptokinase for 1 hour; group 2 (10 rabbits, 10 eyes, 19 vessels) was treated with an infusion in an ear vein of 25 000 IU/kg streptokinase for 1 hour and was subsequently given pulsed ultrasound directed towards the occluded vessels.
FLUORESCIN ANGIOGRAPHY

Thirty minutes after the laser treatment, fluorescein angiography was performed in order to confirm that the vessels were completely occluded. Sodium fluorescein at a concentration of 25% (250 mg/ml in sterile water) was injected in the ear vein. Fluorescein angiography was performed using the scanning laser ophthalmoscope (Rodenstock, Heidelberg, Germany). Vessels that were only partially occluded were excluded from the study. Twelve hours after the treatment, fluorescein angiography was performed again and the patency of the vessels was evaluated. The evaluation of the patency was performed by two of the authors (JL and JG) in a masked mode. All the pictures used for the evaluation were taken 20–30 seconds after the injection of fluorescein.

ULTRASOUND EXPOSURE

Unfocused piezoelectric transducers (Ceram AB, Lund, Sweden) with a resonance frequency of 1.0 MHz and diameter of 20 mm were used. The transducers were excited by an electronic system consisting of a function generator (HP 3314A, Hewlett-Packard, Washington, USA) and a RF power amplifier (ENI 240L, ENI, Rochester, New York, USA). The output of the function generator was manually set to produce the desired ultrasound characteristics, as described below.

The transducers were calibrated by measuring the total radiation pressure on an ultrasound absorbing material (Ceram AB), using an electronic balance (Precisa 400M, PAG Oerlikon AG, Zurich, Switzerland). In the experiment series, up to three transducers were coupled in parallel. Therefore, measurements were made to verify that the ultrasound output was the same regardless of the number of transducers coupled to the amplifier.

To allow good acoustic coupling between the transducer and the eye, ultrasound transmission gel was used (Aquasonic 100, Parker Laboratories Inc, NJ, USA). Owing to interference phenomena, the ultrasound beam is not uniformly distributed close to the surface of the transducer. To avoid this effecting the experiment, the ultrasound transmission gel was put between the cornea and the transducer. The distance was typically 10 mm between the transducer and the cornea, giving a total distance between the transducer and the vessel of about 25 mm.

Pulsed ultrasound of 1 MHz frequency was used: 100 pulses of 1 W/cm² was sent every millisecond (10% duty cycle), resulting in a spatial average, temporal average intensity of 0.1 W/cm².

Pulsed low energy ultrasound was given during the same period of time that streptokinase was administered—that is, for 1 hour.

The rabbits were killed immediately after the second fluorescein angiography by an intravenous injection of pentobarbbitone.

Results

The patency of the vessels was evaluated 12 hours after the laser treatment with fluorescein angiography. Vessels that were only partially open were considered as closed. Leakage of the fluorescein was noted around the laser treatment site.

In group 1 receiving streptokinase (50 000 IU/kg), all the vessels that had been occluded were open. In group 2, which had only been treated with streptokinase (25 000 IU/kg), 4/19 (21%) of the vessels were open, and in group 3, which was treated with streptokinase (25 000 IU/kg) and ultrasound, 14/22 (64%) of the vessels were open (Fig 1).

We used Fisher’s exact test to assess statistical significance. There is a statistical significant difference between groups 1 and 2 (p<0.0001; two sided), between groups 1 and 3 (p=0.03; two sided), and between groups 2 and 3 (p=0.011; two sided).

Discussion

Thrombolytic treatment with streptokinase or tissue plasminogen activator of retinal vein occlusions in humans has been performed before with fairly good results. The thrombolytic treatment is not widely used today in retinal vein occlusion, because of severe side effects such as haemorrhage. If it was possible to lower the dose of the thrombolytic drug and thus lower the frequency of the side effects, and still maintain good thrombolytic effect by adding therapeutic ultrasound, it is probable that this treatment would be of greater clinical interest.

The results of this study suggest that it is possible to reduce the dose of streptokinase and still retain a good thrombolytic effect by adding ultrasound. It has previously been
shown that streptokinase at a dose of 25 000 IU/kg in the rabbit is insufficient to dissolve an arterial thrombus in the ileofoemoral artery, but when ultrasound was added transcutaneously, 59% of the thrombi were dissolved. In our study a dose of streptokinase of 50 000 IU/kg dissolved 100% of the thrombi in the retinal veins. This shows that it is possible to lyse the experimental thrombi if the streptokinase dose is high enough. When the dose was halved to 25 000 IU/kg, the proportion of lysed thrombi fell to 21%, showing that the lysis of thrombi is dose dependent. When adding ultrasound to the lower dose of streptokinase, we managed to lyse 64% of the thromb, thus showing that pulsed ultrasound is an efficient adjuvant to streptokinase treatment.

In a previous work, we found an intensity “window” for in vitro experiments with ultrasound. The effect of streptokinase induced thrombolysis was more enhanced when combined with ultrasound of the intensity 1 W/cm² than with any other, therefore we chose that intensity for this study. The first two rabbits, which were excluded from the study, were given continuous ultrasound. However, these rabbits developed haemorrhage in the anterior chamber, and the intensity had to be lowered. This was achieved by changing to pulsed ultrasound with a 10% duty cycle, after which no more haemorrhages were seen. Since haemorrhage is a non-acceptable side effect, future studies should be made to find the most beneficial ultrasound intensity.

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