Abstract

Aim—To investigate the reproducibility and sensitivity of the Zeiss retinal vessel analyser, a new method for the online determination of retinal vessel diameters in healthy subjects.

Methods—Two model drugs were administered, a peripheral vasoconstrictor (the α receptor agonist phenylephrine) and a peripheral vasodilator (the nitric oxide donor sodium nitroprusside) in stepwise increasing doses. Nine healthy young subjects were studied in a placebo controlled double masked three way crossover design. Subjects received intravenous infusions of either placebo or stepwise increasing doses of phenylephrine (0.5, 1, or 2 µg/kg/min) or sodium nitroprusside (0.5, 1, or 2 µg/kg/min). Retinal vessel diameters were measured with the new Zeiss retinal vessel analyser. Retinal leucocyte velocity, flow, and density were measured with the blue field entoptic technique. The reproducibility of measurements was assessed with coefficients of variation and intraclass correlation coefficients.

Results—Placebo and phenylephrine did not influence retinal haemodynamics, although the α receptor antagonist significantly increased blood pressure. Sodium nitroprusside induced a significant increase in retinal venous and arterial diameters (p<0.001 each), leucocyte density (p<0.001), and leucocyte flow (p=0.024) despite lowering blood pressure to a significant degree. For venous and arterial vessel size measurements short term coefficients of variation were 1.3% and 2.6% and intraclass correlation coefficients were 0.98 and 0.96, respectively. The sensitivity was between 3% and 5% for retinal veins and 5% and 7% for retinal arteries.

Conclusions—These data indicate that the Zeiss retinal vessel analyser is an accurate system for the assessment of retinal diameters in healthy subjects. In addition, nitric oxide appears to have a strong influence on retinal vascular tone.

Methods

SUBJECTS
The study protocol was approved by the ethics committee of Vienna University School of Medicine and followed the guidelines of the Declaration of Helsinki. Nine healthy male subjects (age range 20–27 years, mean 23.6 (SD 2.0)) and seven healthy female non-smoking volunteers participated in this study after signing written informed consent. Each subject passed a screening examination that included medical history and physical examination, 12 lead electrocardiogram, complete blood count, activated partial thromboplastin time, thrombin time, fibrinogen, clinical chemistry (sodium, potassium, creatinine, uric acid, glucose, cholesterol, triglycerides, alanine aminotransferase, aspartate aminotransferase, γ glutamyltransferase, alkaline phosphatase, total bilirubin, total protein), hepatitis A, B, C, and HIV serology, urine analysis, and a urine drug screen. Subjects were excluded if any abnormality was found as part of the screening unless the investigators considered an abnormality as clinically irrelevant. An ophthalmic examination was performed in each subject before the study day. Inclusion criteria were normal ophthalmic findings, ametropia of less than 3 dioptres, and anisometropia of less than 1 dioptre. In all subjects the right eye was studied.

EXPERIMENTAL DESIGN
The study was performed in a randomised, placebo controlled, balanced three way crossover design. Three study days with washout.
Table 1 Coefficient of variation (CV) and intra-class correlation coefficients (κ) for measurements of venous and arterial diameters with the Zeiss retinal vessel analyser and measurements of retinal leucocyte flow with the blue field entoptic technique. Data are presented for short term and day to day variability.

<table>
<thead>
<tr>
<th></th>
<th>Short term variability</th>
<th>Day to day variability</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>CV (S.D.)</td>
<td>CV (S.D.)</td>
</tr>
<tr>
<td>Venous diameter</td>
<td>1.3 % (0.98)</td>
<td>4.4 % (0.90)</td>
</tr>
<tr>
<td>Arterial diameter</td>
<td>2.6 % (0.96)</td>
<td>5.2 % (0.87)</td>
</tr>
<tr>
<td>Retinal blood flow</td>
<td>11.4 % (0.83)</td>
<td>17.6 % (0.64)</td>
</tr>
</tbody>
</table>

Table 2 Baseline ocular haemodynamic variables at the three study days. Data are presented as means (SEM) (n=9).

<table>
<thead>
<tr>
<th></th>
<th>Day 1</th>
<th>Day 2</th>
<th>Day 3</th>
</tr>
</thead>
<tbody>
<tr>
<td>Venous diameter (arbitrary units)</td>
<td>159 (7)</td>
<td>157 (6)</td>
<td>155 (8)</td>
</tr>
<tr>
<td>Arterial diameter (arbitrary units)</td>
<td>139 (10)</td>
<td>132 (8)</td>
<td>137 (9)</td>
</tr>
<tr>
<td>Leucocyte velocity (arbitrary units)</td>
<td>1.10 (0.09)</td>
<td>1.09 (0.08)</td>
<td>1.03 (0.08)</td>
</tr>
<tr>
<td>Leucocyte density (arbitrary units)</td>
<td>103 (17)</td>
<td>103 (18)</td>
<td>113 (17)</td>
</tr>
<tr>
<td>Leucocyte flow (arbitrary units)</td>
<td>117 (19)</td>
<td>114 (23)</td>
<td>125 (21)</td>
</tr>
</tbody>
</table>

Polak, Dorner, Kiss, et al

Zeiss Retinal Vessel Analyser (RVA)
The Zeiss RVA is a commercially available system which comprises a fundus camera (Zeiss FF 450, Jena, Germany), a video camera, a real time monitor, and a personal computer with an analysing software for the accurate determination of retinal arterial and venous diameters. Retinal vessel diameters are analysed in real time with a maximum frequency of 50 Hz. This means that a maximum of 25 vessel diameter readings can be obtained per second. For this purpose the fundus is imaged onto the charge coupled device chip of the video camera. The consecutive fundus images are digitised using a frame grabber. In addition, the fundus image can be inspected on the real time monitor and, if necessary, stored on a video recorder. Evaluation of the retinal vessel diameters can either be done on line or off line from the recorded video tapes.

Because of the absorbing properties of haemoglobin each blood vessel has a specific transmittance profile. Measurement of retinal vessel diameters is based on adaptive algorithms using these specific profiles. Whenever a specific vessel profile is recognised the RVA is able to follow this vessel as long as it appears within the measurement window. This means that the system is able to automatically correct for alterations in luminance as induced, for instance, by slight eye movements. If the requirements for the assessment of retinal vessel diameters are not being fulfilled, as occurs during blinking, the system automatically stops the measurement of vessel diameter. As soon as an adequate fundus image is achieved again, measurement of vessel diameters restarts automatically.

To select a region of interest the user defines a rectangle on the screen of the real time monitor. This window can either include a retinal artery or a retinal vein or both. Thereafter the measurement of vessel diameters can be started. Retinal vessel diameter is then calculated along the arterial or venous segment, which lies within the rectangle. If the region of interest consists of an artery and a vein, both vessel diameters are recorded simultaneously. As long as the vessels under study are within the selected rectangle the system automatically corrects for eye movements. This is made possible by the adaptive nature of the diameter analysis. Hence vessel diameter can be recorded as a function of time as well as a function of the position along the vessel. In contrast with other procedures, which have been proposed for the determination of retinal vessel size, this system measures diameters only in relative units.

Blue Field Entoptic Technique
This non-invasive method is described in detail by Riva and Petrig. The blue field entoptic phenomenon can best be seen by looking into a blue light with a narrow optical spectrum at a wavelength of approximately 430 nm. Under these conditions corpuscles can be seen moving in an area of 10–15 degrees of arc radius centred at the fovea. Most probably this phenomenon is caused by the fact that red, but not white, blood cells absorb short wavelength light. Thus the passage of a white blood cell is perceived as a flying corpuscle. For determination of retinal haemodynamic parameters a stimulated particle field is shown to the subjects under study. By comparison with their own entoptic observation subjects can adjust the number of white blood cells and the mean flow velocity from which the retinal leucocyte flow can be calculated. In the present studies at least five matching trials were performed by each subject. Only values with a coefficient of variation of less than 15% were considered accurate. Subjects who did not reach the required reproducibility were excluded from the study.
Systolic, diastolic, and mean blood pressures (SBP, DBP, MAP) were measured on the upper arm by an automated oscillometric device (HP-CMS patient monitor, Hewlett Packard, Palo Alto, CA, USA). Pulse rate (PR) was automatically recorded from a finger pulse oxymetric device (HP-CMS patient monitor).

DATA ANALYSIS
To quantify the short term variability and the day to day variability of the measurements intraclass correlation coefficients (κ) for retinal venous and arterial diameters measured with the Zeiss retinal vessel analyser, as well as for retinal leucocyte flow measured with the blue field entoptic technique, were calculated. The calculation of κ is based on a repeated measure ANOVA model using the variance among subjects (vs), the variance among measurements (vm), and the residual error variance (ve):

\[
\kappa = \frac{(vs - ve)}{(vs + ve + 2 \times vm)}
\]

The higher the intraclass correlation coefficients the better the reproducibility of the method. A κ of 1 reflects perfect reproducibility. The intraclass correlation coefficient is a generally accepted measure of reliability and is considered more appropriate than older methods, such as \(\chi^2\), percentage agreement, product moment correlation, or Yule's Y. Short term variability (κs) was calculated from the four measurements performed on the placebo study day. Day to day variability (κd) was calculated from the baseline measurements of the three study days. As an additional measure of variability, the coefficient of variation, was calculated for short term and day to day data. For this purpose individual coefficients of variation were calculated from the four readings at the placebo day and the three baseline readings of the three study days, respectively. The mean of these individual data are presented.

Effects of the haemodynamic model drugs were assessed by repeated measure ANOVA versus placebo and by repeated measure ANOVA versus baseline. Post hoc comparisons were done using paired \(t\) tests and Bonferroni's correction for multiple comparisons. For data description drug induced changes were expressed as percentage change from baseline. Results are given as mean (SEM). \(p < 0.05\) was considered the level of significance.

Results
The intraclass correlation coefficients and the coefficients of variation for the measurement of retinal haemodynamic variables are presented in Table 1. Short term measurements of retinal vessel diameters with the Zeiss retinal vessel analyser were performed on the placebo study day.

<table>
<thead>
<tr>
<th></th>
<th>Systolic blood pressure (mm Hg)</th>
<th>Diastolic blood pressure (mm Hg)</th>
<th>Pulse rate (beats/min)</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Placebo day</strong></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Baseline</td>
<td>114.5 (9.2)</td>
<td>60.9 (7.4)</td>
<td>70.7 (10.3)</td>
</tr>
<tr>
<td>Syringe 1</td>
<td>113.4 (7.6)</td>
<td>61.1 (5.4)</td>
<td>68.6 (11.6)</td>
</tr>
<tr>
<td>Syringe 2</td>
<td>112.9 (3.3)</td>
<td>60.8 (6.5)</td>
<td>67.3 (8.8)</td>
</tr>
<tr>
<td>Syringe 3</td>
<td>109.6 (11.1)</td>
<td>59.9 (6.9)</td>
<td>67.2 (10.6)</td>
</tr>
<tr>
<td><strong>Phenylephrine</strong></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Baseline</td>
<td>113.8 (8.5)</td>
<td>57.8 (9.2)</td>
<td>61.2 (5.9)</td>
</tr>
<tr>
<td>0.5 µg/kg/min</td>
<td>121.0 (9.2)</td>
<td>62.5 (10.9)</td>
<td>59.2 (9.5)</td>
</tr>
<tr>
<td>1.0 µg/kg/min</td>
<td>132.5 (11.0)</td>
<td>69.1 (10.4)</td>
<td>48.9 (8.3)</td>
</tr>
<tr>
<td>2.0 µg/kg/min</td>
<td>145.4 (12.6)</td>
<td>81.5 (11.1)</td>
<td>45.9 (7.6)</td>
</tr>
<tr>
<td><strong>Sodium nitroprusside</strong></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Baseline</td>
<td>113.7 (8.4)</td>
<td>61.2 (5.9)</td>
<td>70.8 (6.1)</td>
</tr>
<tr>
<td>0.5 µg/kg/min</td>
<td>101.5 (11.9)</td>
<td>59.2 (9.5)</td>
<td>71.6 (6.8)</td>
</tr>
<tr>
<td>1.0 µg/kg/min</td>
<td>98.9 (9.7)</td>
<td>48.9 (8.3)</td>
<td>80.1 (12.7)</td>
</tr>
<tr>
<td>2.0 µg/kg/min</td>
<td>96.6 (6.5)</td>
<td>45.6 (7.6)</td>
<td>83.0 (6.7)</td>
</tr>
</tbody>
</table>

Figure 1 Effect of stepwise increasing doses of placebo (broken lines), phenylephrine, or sodium nitroprusside (solid lines) on retinal venous and arterial diameter. Data are presented as means (SEM) \((n = 9)\). At the highest dose of phenylephrine and sodium nitroprusside only seven subjects were eligible for analysis. Asterisks indicate significant changes versus placebo.

Table 3 Effects of placebo (physiological saline solution) or stepwise increasing doses of sodium nitroprusside, or phenylephrine on systolic and diastolic blood pressure and pulse rate. Data are presented as means (SEM) \((n=9)\)

<table>
<thead>
<tr>
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Figure 1 Effect of stepwise increasing doses of placebo (broken lines), phenylephrine, or sodium nitroprusside (solid lines) on retinal venous and arterial diameter. Data are presented as means (SEM) \((n = 9)\). At the highest dose of phenylephrine and sodium nitroprusside only seven subjects were eligible for analysis. Asterisks indicate significant changes versus placebo.
and sodium nitroprusside only seven subjects were eligible for analysis. Asterisks indicate significant changes versus placebo.

Figure 2  Effect of stepwise increasing doses of placebo (broken lines), phenylephrine, or sodium nitroprusside (solid lines) on leucocyte velocity, density of leucocytes, and leucocyte flow. Data are presented as means (SEM) (n = 9). At the highest dose of phenylephrine sodium nitroprusside (solid lines) on leucocyte velocity, density of leucocytes, and leucocyte flow (p<0.021), but not versus placebo. The effect of 1 µg/kg/min sodium nitroprusside (5.4% (0.4%)) was highly significant versus baseline and placebo (p<0.001 each). The effect of the lowest dose of sodium nitroprusside on retinal venous diameter (3.0% (0.8%)) was significant versus baseline (p=0.023), but not versus placebo. The effect of 1 µg/kg/min sodium nitroprusside on retinal arterial diameter (4.5% (1.5%)) was again significant versus baseline (p=0.021), but not versus placebo. The effect of 1 µg/kg/min sodium nitroprusside on retinal arterial diameter (6.8% (1.6%)) was significant versus baseline (p=0.002) and placebo (p=0.015). Sodium nitroprusside also induced a dose dependent increase in retinal leucocyte flow (p=0.024, Fig 2). This effect was caused by an increase in retinal leucocyte density (p=0.001), whereas retinal leucocyte velocity was virtually unchanged by the nitric oxide donor.

Discussion

The main purpose of the present study was to investigate the reproducibility and sensitivity of retinal vessel diameter measurements with the new Zeiss retinal vessel analyser. Our results indicate that the reproducibility in healthy subjects is higher for retinal veins than for retinal arteries. This could be a resolution size phenomenon, because in comparable fundus locations the veins are larger than the arteries. In addition, this may be related to the more pulsatile blood flow in the arterial tree, which leads to more pronounced vessel diameter changes during the cardiac cycle. ECG triggering may therefore reduce short term variability of retinal vessel measurements with the Zeiss retinal vessel analyser. Nevertheless we obtained high short term reproducibility for vessel size determinations in both arteries and veins in the present trial. Day to day reproduc-
The sensitivity of vessel size determinations with the Zeiss retinal vessel analyser was investigated using two model drugs in the present study. Our data indicate that in a double masked placebo controlled crossover trial in nine healthy subjects changes between 3% and 5% in retinal venous diameters and changes between 5% and 7% in arterial diameters can be detected with this system. As retinal blood flow is dependent on the cross sectional area of the vessel our data indicate that changes in retinal blood flow in the order of 6–10% and 10–14% are detectable if measurements are taken from retinal veins and arteries, respectively. However, for a calculation of blood flow from retinal veins and arteries, respectively. However, for a calculation of blood flow obtained with these two techniques, one has to consider that an approximately 10% increase in vessel diameter indicates an approximately 20% increase in retinal blood flow through the major vessels, if blood velocity is assumed constant.

In conclusion we have shown that the Zeiss retinal vessel analyser provides a satisfactory reproducibility and sensitivity for pharmacodynamic studies. In addition, our data indicate that nitric oxide is a potent vasodilator in human retinal vessels.

The authors thank Zeis Jena for the loan of the Zeiss RVA system. Particularly we thank Werner Infanger from Zeiss Vienna for his support. In addition, we thank Walter Vilsen and Thomas Riemer for their extensive introduction to the operation of the RVA. Excellent assistance from Susan Emichner, RN, and Ursula Graselli, RN, is acknowledged.


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Evaluation of the Zeiss retinal vessel analyser

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