Ocular blood flow alteration in glaucoma is related to systemic vascular dysregulation

M Emre, S Orgül, K Gugleta, J Flammer

Aims: To investigate the source of ocular blood flow alterations in glaucoma.

Methods: In 56 patients with open angle glaucoma, blood flow parameters were obtained from both eyes in the ocular circulation and the choroidal circulation by means of colour Doppler imaging, as well as in the choroidal circulation and the neuroretinal rim of the optic nerve by means of laser Doppler flowmetry. Based on these haemodynamic parameters, a cluster analysis (two groups) was performed and differences with regard to risk factors were assessed between clusters.

Results: Ocular blood flow data in the two clusters indicated that the two groups (cluster 1 = 26 patient with higher blood flow values; cluster 2 = 30 patients with lower blood flow values) differed mainly in choroidal and optic nerve blood flow. No differences in sex distribution, propensity to have normal tension glaucoma, age, endothelin-1 plasma levels, visual field damage, intraocular pressure, or systemic blood pressure parameters were observed between the two clusters. However, 12 patients (46%) from the cluster with high ocular blood flow values showed a vasospastic response in nailfold capillaroscopy, while such a response was observed in 24 patients (80%) of the cluster with low ocular blood flow values. This difference in vasospastic propensity was statistically significant (p = 0.0121).

Conclusions: Ocular blood flow alterations in glaucoma patients seem, at least partly, to be related to a systemic vascular dysregulation.
had 3 mm or larger pupil diameters when their fields were plotted.

**Systemic blood pressure**
All patients had a 24 hour blood pressure monitor (Mobil-O-Graph, IEM GmbH, Stolberg, Germany). During daytime (from 8 am to 10 pm) and nighttime (from 10 pm to 8 am) the measurement intervals were 30 minutes. Recordings were performed in the hospital, so that the patients were all under comparable conditions during the 24 hour blood pressure measurement period. The mean systolic (SBP), and diastolic blood pressure (DBP) for daytime and nighttime were computed for each patient. The blood pressure dip, representing the fall in blood pressure during nighttime expressed as a percentage of the average daytime reading level, was determined for SBP and DBP in each patient. Using average IOP of the diurnal tension curve and mean SBP and DBP during daytime, ocular perfusion pressure (OPP) was estimated for each eye (OPP = \( \frac{1}{3} \times [\frac{1}{5} \text{DBP} + \frac{1}{5} \text{SBP} – \text{IOP}] \)).

**Nailfold capillaroscopy**
All the patients underwent microscopic examination of their nailfold capillaries, as described previously. Briefly, a light microscope is coupled to a television monitor that is in turn coupled to a video recorder, allowing the observed blood flow to be videotaped for later analysis. During capillaroscopy, the nailfold area is cooled to -15°C for 60 seconds by rapidly decompressing carbon dioxide. The examination is performed in a room with a constant temperature of about 23°C (range 21°C–25°C). During cooling, the blood in the capillaries sometimes stops flowing. Digital vasospasm is defined as a closing of one or more visible capillaries, with a mean stoppage time of longer than 12 seconds.

**Colour Doppler sonography**
All the glaucoma patients underwent blood flow velocity assessment of their ophthalmic artery (OA) and their central retinal artery (CRA) by means of colour Doppler imaging (CDI) as described previously. The same experienced sonographer performed all retrobulbar CDI examinations by means of a colour Doppler imaging device (Siemens Albris AG, Zürich, Switzerland) using a 7.5 MHz linear phase array transducer. During the examination, patients were in the supine position, with the upper body tilted upward at about a 30 degree angle. In each vessel, peak systolic velocity (PSV), defined as the highest velocity of blood flow during the systolic phase of the cardiac cycle and the end diastolic velocity (EDV), defined as the velocity of blood flow at the end of the diastolic phase of the cardiac cycle were measured in both eyes of each glaucoma patient. Throughout the entire experimental procedure, systemic blood pressure and heart rate were recorded at 3 minute intervals by means of an automatic device (Mobil-O-Graph, IEM GmbH, Stolberg, Germany). Readings obtained during relevant variations in blood pressure were excluded.

**Blood flow measurement in the neuroretinal rim of the optic nerve**
Blood flow in the neuroretinal rim of the optic nerve was determined using laser Doppler flowmetry technique (LDF). The patients were seated in front of a Topcon fundus camera (Model TRC, Topcon; Tokyo, Japan). The instrument (laser Doppler flowmeter, Oculix SA, Arbaz, Switzerland) contains three light sources: a probing laser beam (wavelength: 670 nm; power: 26 μW) for measurement (lasting 10–20 seconds, the power was well within the 1986 ANSI Z136.1 American National Standard of 107 μW for a 20 minute exposure and 25 μW for infinite exposure at this wavelength), a red free annulus of light to illuminate the fundus for viewing, and a fixation target. The fixation target is a 670 nm diode laser coupled to an optical fibre on a micromanipulator stage that allows positioning of the optic disc in the centre of the visible field.

The fundus camera was adjusted to produce an evenly illuminated focused view of the fundus. The probing laser beam was positioned with a rotatable biprism to pass through the inferior sector of the pupil and was focused to a distinct spot of −160 μm in diameter on the temporal inferior neuroretinal rim, a relatively large area with good chances to allow such a measurement, distant from large calibre vessels. Patients with much damage to the temporal inferior neuroretinal rim precluding proper measurement in neural tissue were excluded. The fixation target was used to position the subject’s fundus relative to the probing laser beam. An optical fibre detector with an effective 160 μm diameter aperture located in the optic disc image plane of the fundus camera was positioned over the image of the spot illuminated by the probing laser beam. The detector collects the laser light scattered from the optic disc (Doppler shifted and non-shifted light) and delivers it to an external photomultiplier tube. A continuous real time digital signal processor calculates the fast Fourier transformed power spectrum. Blood flow parameters were determined by analysing the LDF signal with a NeXT (Redwood City, CA, USA) computer, using an algorithm (BPM403A, Vasamedics, Minneapolis; PeriFlux PF3, Perimed, Stockholm, Sweden) based on Bonner and Nossal’s photon diffusion theory. The calculated parameters (velocity, volume, and flux) are based on blood particle velocity and are related to each other through the relationship flux = constant × volume × velocity. Each parameter, although given in arbitrary units, varies linearly with respect to changes in blood flow.

**Blood flow measurement in the choroid**
Choroidal blood flow was also determined using a method based on the laser Doppler flowmetry technique. A new device able to measure subfoveal choroidal blood flow in the fovea has been developed. The optical system is based on a confocal arrangement. A polarised laser source (λ = 785 nm, 100 m) is relayed with a 1:1 optical system (laser beam at the cornea: width = 1.3 mm, power = 90 μW) and focused at the subject’s retina (spot in the retinal image plane = 10–20 μm in diameter, optical thickness of confocal layer = 300 μm). The point laser source, the point of illumination of the fovea, and the detecting optical fibre are located in conjugated planes. The scattered light is collected by an optical system organised with six fibres arranged circularly around the central fixation point along a circle of diameter of 180 μm (within the avascular zone of the fovea). The photocurrent from the photodetector is Fourier transformed and the haemodynamic parameters flux, volume, and velocity are processed as outlined above. As for optic nerve laser Doppler flowmetry, each parameter varies linearly with respect to changes in blood flow.

The subjects fixated the red light spot within the oculus and adjusted the focus by turning the oculus. The oculus to cornea distance was set between 1.5 and 2 cm. A constant very low level artificial room illumination was used throughout all the experiments. A stable DC during a recording was used as a criterion of proper fixation. One measurement of 10–20 seconds was obtained for each eye. Again, only the parameter flux was considered for further analysis.
Statistics

The blood pressure monitoring, the diurnal IOP curve, the CDI and laser Doppler measurements were obtained during the same 24 hour interval for each patient. Haemodynamic parameters were studied after a light breakfast and patients were asked to refrain from alcohol and caffeine for 12 hours before the measurements. A resting period of at least 30 minutes was scheduled before each haemodynamic measurement. Each time, stable baseline conditions were established, based on repeated measurements of blood pressure. Based on ocular blood flow data (one parameter per vascular bed in each eye: EDV in the ophthalmic artery and the central retinal artery as well as the LDF parameter flux of the neuroretinal rim of the optic nerve and the choroid) from both eyes of each patient, two distinct groups were computed by means of cluster analysis (Statistics for Windows, StatSoft Inc, Tulsa, OK, USA). The multivariate computation in a cluster analysis allows taking into account the influence of related variables, such as data from the fellow eye. Differences between the two clusters in age, visual field damage (index ‘mean defect’), peak and average IOP during the diurnal tension curve, systemic blood pressure, average ocular perfusion pressure, endothelin-1 plasma level, were evaluated by the t test for independent variables. Differences in sex distribution, propensity to have normal tension glaucoma (peak IOP: <21 mm Hg in the diurnal tension curve) or to be vasospastic (positive nailfold capillaroscopy) were evaluated by the Fisher exact test. Differences were considered statistically significant at p <0.05.

RESULTS

Among the 56 glaucoma patients, cluster analysis grouped 26 patients (18 women and eight men) in a first group with higher blood flow parameters (cluster 1) and 30 patients (19 women and 11 men) in a second group with lower blood flow parameters (cluster 2). Ocular blood flow data in these two clusters are displayed in table 1. The data indicate that the two groups differed mainly in choroidal and optic nerve blood flow (fig 1). The sex distribution was statistically comparable between the two groups (Fisher’s exact test: p = 0.78). The mean age was 66 (SD 17) years for the group with high ocular blood flow values (cluster 1) and 66 (12) years for the 30 patients (cluster 2) showing low ocular blood flow values (p = 0.89). Endothelin-1 plasma levels, visual field damage, peak and average IOP during diurnal tension curve, systemic blood pressure parameters, and ocular perfusion values did not show statistically significant differences between the two groups (table 2). Twelve patients from the first cluster and 11 patients of the second cluster had normal tension glaucoma (p = 0.59). In contrast, while 12 patients (46%) from the first cluster (high ocular blood flow values) showed a vasospastic response in nailfold capillaroscopy, such a response was observed in 24 patients (80%) from the cluster with low ocular blood flow values (p = 0.0121).

DISCUSSION

Two clusters of patients with open angle glaucoma were computed based on ocular blood flow parameters. Although some uncertainty regarding the nature of the parameters measured with the devices used in the present study persists,23 all are related to ocular blood flow. In the present study, the two computed groups differed mainly in choroidal and optic nerve blood flow parameters. Between these two clusters, no differences in sex distribution, propensity to have normal tension glaucoma, age, endothelin-1 plasma levels, visual field damage, intraocular pressure, systemic blood pressure parameters, or ocular perfusion values were observed. The only statistically significant difference between the two groups, besides the parameters used to compute the two clusters, was the propensity to show a vasospastic response in nailfold capillaroscopy, with 46% of the patients of the group with high values of ocular blood flow parameters showing a capillary blood flow stop, while this proportion reached 80% among the patients with low values of ocular blood flow parameters. The present study did not address the effect of low values of blood flow parameters on the

![Figure 1](image-url)

**Figure 1** Based on ocular blood flow parameters two groups were computed by means of a cluster analysis. The two groups differed mainly in choroidal and optic nerve blood flow. *Indicates significantly different parameters; ophthalmic artery stays for end diastolic velocity in the ophthalmic artery of the right and left eyes respectively; retinal artery stays for end diastolic velocity in the central retinal artery of the right and left eyes respectively; choroid stays for the choroidal laser Doppler flowmetry parameter flux in the right and left eyes respectively; optic nerve stays for the optic nerve laser Doppler flowmetry parameter flux in the right and left eyes, respectively. The variables were standardised for the mean value among the 56 glaucoma patients. The boxes represent the standard error of the mean and the whiskers represent the standard deviation.

<table>
<thead>
<tr>
<th>Table 1 Ocular haemodynamic parameters (mean (SD))</th>
</tr>
</thead>
<tbody>
<tr>
<td>Cluster 1 (26 patients)</td>
</tr>
<tr>
<td>EDV (cm/s) in the right ophthalmic artery</td>
</tr>
<tr>
<td>EDV (cm/s) in the left ophthalmic artery</td>
</tr>
<tr>
<td>EDV (cm/s) in the right central retinal artery</td>
</tr>
<tr>
<td>EDV (cm/s) in the left central retinal artery</td>
</tr>
<tr>
<td>Choroidal flux (AU) in the right eye</td>
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<tr>
<td>Choroidal flux (AU) in the left eye</td>
</tr>
<tr>
<td>Optic nerve flux (AU) in the right eye</td>
</tr>
<tr>
<td>Optic nerve flux (AU) in the left eye</td>
</tr>
</tbody>
</table>

EDV = colour Doppler parameter end diastolic velocity; AU = arbitrary units.
prognosis of glaucomatous disease, but suggested a statistical association between altered ocular blood flow parameters and a vasospastic propensity. This observation is of importance, indicating that systemic blood flow alterations are related to ocular blood disturbances in glaucoma.

We used a somewhat unusual approach in the present analysis. In contrast with traditional hypothesis testing designed to verify differences between groups of patients, an exploratory data analysis was employed. Parameters of ocular blood flow were used to compute two groups, using cluster analysis, a multivariate exploratory technique designed specifically to identify patterns in multivariate data sets. Theoretically, any set of variables such as intraocular pressure or visual field damage can be used to compute clusters, each approach addressing a different question.

Computationally, cluster analysis may be thought of as analysis of variance “in reverse.” The computation will start with random clusters, and then move patients between those clusters with the goal to (1) minimise variability within clusters and (2) maximise variability between clusters. In contrast with traditional hypothesis testing where groups of patients are defined based on obvious criteria, a cluster analysis allows us to define groups of patients based on more complex characteristics. Once the groups are defined, they can be compared with regard to parameters other than those used to compute the clusters.

The present cluster analysis yielded intriguing observations. The most marked differences were noted for choroidal and optic nerve blood flow parameters (both eyes showing the same trend). End diastolic velocity in the ophthalmic artery (probably the least “ocular” of all tested vessels) was higher, but only borderline significantly and only in the left eyes of patients with generally low ocular blood flow. Therefore, this finding does, in our opinion, not invalidate our consideration of the two clusters as one group with low ocular blood flow and one group with high ocular blood flow. Patients with low values of ocular blood flow parameters did not have more advanced visual field damage, suggesting that blood flow alterations do not, at least not only, occur secondary to visual field damage. The same patients were not necessarily patients with normal tension glaucoma and did not have markedly lower untreated IOP readings in a diurnal tension curve, suggesting that ocular blood flow alterations are not, at least not only, secondary to increased IOP. Furthermore, low values of ocular blood flow parameters were not related to low systemic blood pressure, suggesting that ocular blood flow alterations occur not only in response to systemic perturbations. The only positive association with low values of ocular blood flow parameters was observed with a vasospastic responsiveness of the nailfold capillaries. The fact that up to half of the patients with high values of ocular blood flow parameters show a vasospastic responsiveness of the nailfold capillaries suggests that the presence of systemic vasospastic responsiveness does not necessarily mean that ocular blood flow is altered. This is also in accordance with the relative high frequency of a vasospastic propensity in a healthy population. Nevertheless, the fact that four out of five patients with low values of ocular blood flow parameters showing a vasospastic responsiveness of the nailfold capillaries, suggests an association between altered ocular blood flow and vasospastic propensity. It is unlikely that the latter association is because the observed lower values of ocular blood flow parameters are brought about by a systemic vasocostrictive response to an external perturbation. However, although this interpretation is purely speculative, it is possible that similar phenomena occur within the ocular vascular bed of some, but not all, glaucoma patients with a vasospastic responsiveness of the nailfold capillaries, leading ultimately to lower blood flow parameters. Most importantly, results of a cluster analysis are to be understood as giving a hunch of what should be investigated. An inferring interpretation of the results would not be appropriate and the present findings need further confirmation.

Regarding risk factors in glaucoma, the differentiation between mechanical damage, as a consequence of IOP, and vascular theories, considering glaucomatous optic neuropathy as a consequence of insufficient blood supply, had little therapeutic impact so far, as IOP reduction was the only intervention available for treatment of glaucoma. Clinical intervention studies have proved the role of IOP and the benefits of IOP lowering treatment. Given the success of IOP reduction, consideration of ancillary risk factors may seem distracting. However, once pharmacological means and laser surgery have failed, what remains is a filtering procedure with all its risks and possible complications. Elucidating how other factors influence the course of glaucomatous disease may open new therapeutic avenues as well as surgical treatment.

**Table 2** Endothelin-1 plasma levels, visual field damage, intraocular pressure, and systemic blood pressure (mean (SD))

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Cluster 1 (26 patients)</th>
<th>Cluster 2 (30 patients)</th>
<th>p Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Endothelin-1 plasma level (pg/ml)</td>
<td>2.90 (0.76)</td>
<td>2.90 (0.81)</td>
<td>0.98</td>
</tr>
<tr>
<td>MD in left eyes (dB)</td>
<td>7.65 (6.87)</td>
<td>7.95 (6.63)</td>
<td>0.87</td>
</tr>
<tr>
<td>MD in right eyes (dB)</td>
<td>8.32 (7.29)</td>
<td>10.36 (18.65)</td>
<td>0.60</td>
</tr>
<tr>
<td>Peak IOP in left eyes (mm Hg)</td>
<td>21.88 (6.50)</td>
<td>21.50 (5.12)</td>
<td>0.81</td>
</tr>
<tr>
<td>Peak IOP in right eyes (mm Hg)</td>
<td>21.37 (7.50)</td>
<td>21.37 (4.35)</td>
<td>0.61</td>
</tr>
<tr>
<td>Average IOP in left eyes (mm Hg)</td>
<td>14.63 (2.00)</td>
<td>14.37 (2.78)</td>
<td>0.70</td>
</tr>
<tr>
<td>Average IOP in right eyes (mm Hg)</td>
<td>14.61 (3.47)</td>
<td>14.87 (2.85)</td>
<td>0.76</td>
</tr>
<tr>
<td>Average systolic 24 hours blood pressure (mm Hg)</td>
<td>118.71 (19.04)</td>
<td>118.72 (18.23)</td>
<td>0.99</td>
</tr>
<tr>
<td>Average diastolic 24 hours blood pressure (mm Hg)</td>
<td>74.04 (9.68)</td>
<td>74.04 (9.81)</td>
<td>0.99</td>
</tr>
<tr>
<td>Average systolic day-time blood pressure (mm Hg)</td>
<td>128.66 (20.29)</td>
<td>127.95 (17.41)</td>
<td>0.89</td>
</tr>
<tr>
<td>Average diastolic day-time blood pressure (mm Hg)</td>
<td>81.69 (9.98)</td>
<td>81.18 (9.27)</td>
<td>0.85</td>
</tr>
<tr>
<td>Average systolic night-time blood pressure (mm Hg)</td>
<td>111.59 (18.50)</td>
<td>112.60 (20.38)</td>
<td>0.85</td>
</tr>
<tr>
<td>Average diastolic night-time blood pressure (mm Hg)</td>
<td>68.51 (9.49)</td>
<td>69.28 (11.41)</td>
<td>0.79</td>
</tr>
<tr>
<td>Nocturnal drop (%) of systolic blood pressure</td>
<td>13.15 (5.90)</td>
<td>12.04 (8.94)</td>
<td>0.59</td>
</tr>
<tr>
<td>Nocturnal drop (%) of diastolic blood pressure</td>
<td>15.99 (7.71)</td>
<td>14.60 (10.33)</td>
<td>0.58</td>
</tr>
<tr>
<td>Ocular perfusion pressure in right eyes</td>
<td>50.27 (7.35)</td>
<td>50.14 (7.47)</td>
<td>0.95</td>
</tr>
<tr>
<td>Ocular perfusion pressure in left eyes</td>
<td>50.29 (7.84)</td>
<td>49.64 (7.23)</td>
<td>0.75</td>
</tr>
</tbody>
</table>

MD = visual field index "mean defect"; IOP = intraocular pressure; values refer to values obtained during the diurnal tension curve; blood pressure values refer to values obtained during 24 hour blood pressure monitoring.

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REFERENCES
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