Radioactive eye plaques are typically positioned on the sclera to cover the intraocular tumour base and a 2–3 mm free margin of normal-appearing tissue. However, this is not possible in treatment of tumours that touch or surround the optic disc. This is because the optic nerve exits the posterior aspect of the globe, creating an obstacle to proper plaque placement. In addition, the retrobulbar optic nerve sheath diameter is typically three times that of the optic disc. Therefore, even when a notched plaque is perfectly placed against the optic nerve sheath, the plaque’s posterior edge is likely to be at least 1.7 mm anterior to the optic disc and the plaque’s posterior margin extends beyond the optic disc. Thus, as the nerve entered the slot, the plaque’s posterior margin extended beyond the optic disc.

Despite this anatomical handicap, plaque radiation therapy has offered local control of selected juxtapapillary tumours. In these cases, plaque notching, radiation side-scatter and posterior “plaque tilting” have been suggested as factors that allow successful treatment. Intraoperative ultrasonographic or specialised plaque-localisation techniques are recommended. However, most eye cancer specialists will currently recommend enucleation or external beam irradiation of eyes with tumours in contact with ≥180° of the optic disc. Plaque radiation therapy for tumours that touch or surround the optic disc continues to be a clinical challenge.

This study demonstrates how juxtapapillary and even circumpapillary tumours can be treated with radioactive plaques. Finger’s “slotted”-plaque design reduces the probability of geographical miss by allowing the entire optic nerve (and a 2 mm free margin of safety) to be incorporated beneath the plaque.

**MATERIALS AND METHODS**

**Plaque construction**

The goal of slotted-plaque construction was to incorporate at least a portion of the retrobulbar optic nerve within the plaque. Plaque shells were altered to create an 8 mm-wide (transverse diameter) slot at their posterior margin (fig 1). The depth (longitudinal diameter) of the slot was modulated to include the tumour and a 2–3 mm margin of normal-appearing tissue beyond its posterior margin.

Table 1 and figure 2 demonstrate four hypothetical tumours with varying degrees of involvement of the optic disc. Comparative dosimetry was performed to estimate the relative dose distributions to the tumour, centre of the optic nerve and fovea using palladium-103 (Pd103), iodine-125 (I125) and ruthenium-106 (Ru106). When possible, a nasal approach will decrease irradiation of the fovea. Calculations were performed and images created using the Plaque Simulator Software Program (Bebig, Berlin, Germany).

**Calculation of Slot Depth**

**Optic nerve sheath distance**

Optic nerve sheath distance is defined as the (anterior–posterior) distance between the horizontal edge of the optic disc and the optic nerve sheath. For example, optic nerve sheath distance can be estimated based on a mean 5 mm optic nerve sheath diameter—a mean 1.63 mm (1.5 horizontal or 1.75 vertical) optic disc diameter divided by 2 = 1.7 mm.

**Slot depth calculation**

Using this 1.7 mm optic nerve sheath distance, add 0.75 mm (half the horizontal optic disc diameter) and a 3.0 mm (tumour-free margin) and a measured millimetre value of tumour extension beyond the disc midline = slot depth.

**Hypothetical Example**

A calculation used to decide the slot depth for treatment of a tumour in contact with 180° of the optic disc could be approximated as follows: 1.7 mm (optic nerve sheath distance) and 0.75 mm (half-thickness of optic disc because of 180° perineural tumour extension) and 3.0 mm of additional posterior margin. Simple addition results in a 5.5 mm slot depth (depending on the preferred amount of tumour-free posterior margin).

In practice, the actual optic disc and optic nerve sheath diameter were measured with fundus photography and three-dimensional ultrasound C-scan techniques. For ease of plaque insertion (access to the plaque eyelets), at least 10 mm of plaque diameter was retained from the apex of the slot, along the longitudinal axis towards the anterior margin.
and eyelets (fig 1). These requirements limited plaque diameters to >16 mm (table 1).

Slot depth +10 mm = overall plaque diameter

**Slotted-plaque dosimetry**

To maximise the tumour dose and minimise irradiation of normal ocular structures, radioactive seeds were manually affixed within the plaque. The distribution of radioactive seeds was adjusted to conform to tumour size and location and to compensate for the gap created by the slot. Seed locations were documented and digitised. In this series, a minimum tumour dose of 85 Gy was prescribed to an axial depth of >5 mm. Thus, the prescription point (at depth) can be modulated to provide a minimum tumour tissue dose.

For illustration, dosimetry is presented using the Plaque Simulator Program; radiation dosimetry simulations were performed to compare the dose distributions provided by slotted-plaque designs (using Pd-103, I-125 or Ru-106) (table 1).17–19

**Plaque insertion**

Slotted eye plaques can be inserted much like other eye plaques. However, temporary disinsertion of both rectus and oblique muscle was more probably required (two of three cases). Owing, in part, to juxtapapillary positioning and posterior

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**Table 1** Finger’s slotted plaque radiation therapy

<table>
<thead>
<tr>
<th>Example of tumours</th>
<th>Plaque size</th>
<th>Slot width</th>
<th>Slot length</th>
<th>Source</th>
<th>Dose (tumour)</th>
<th>Prescription (point–axial)</th>
<th>Dose (optic disc)</th>
<th>Dose (fovea)</th>
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<tbody>
<tr>
<td>Juxtapapillary</td>
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<td>16</td>
<td>8</td>
<td>6</td>
<td>Pd-103</td>
<td>85</td>
<td>5</td>
<td>167.9</td>
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<tr>
<td>10 x 10 x 5</td>
<td>16</td>
<td>8</td>
<td>6</td>
<td>I-125</td>
<td>85</td>
<td>5</td>
<td>135.9</td>
<td>64.9</td>
</tr>
<tr>
<td>10 x 10 x 5</td>
<td>16</td>
<td>8</td>
<td>6</td>
<td>Ru-106</td>
<td>85</td>
<td>5</td>
<td>64.4</td>
<td>8.5</td>
</tr>
<tr>
<td>Barely circumpapillary*</td>
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<td>18</td>
<td>8</td>
<td>8</td>
<td>Pd-103</td>
<td>85</td>
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<td>144.9</td>
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<td>12 x 12 x 5</td>
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<td>I-125</td>
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<td>68.7</td>
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<tr>
<td>12 x 12 x 5</td>
<td>18</td>
<td>8</td>
<td>8</td>
<td>Ru-106</td>
<td>85</td>
<td>5</td>
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<td>8</td>
<td>10</td>
<td>I-125</td>
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<tr>
<td>14 x 14 x 5</td>
<td>20</td>
<td>8</td>
<td>10</td>
<td>Ru-106</td>
<td>85</td>
<td>5</td>
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<tr>
<td>Largely circumpapillary</td>
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<tr>
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<td>220.4</td>
</tr>
</tbody>
</table>

I, iodine; Pd, palladium; Ru, ruthenium.

*See fig 2c.

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**Figure 1** Finger’s slotted eye plaque radiation therapy: External photographs (A, B) reveal two perspectives of an 18 mm slotted plaque. This slotted plaque retains a 10 mm longitudinal plaque diameter from the slot apex to the anterior “eyelet” margin. It also contains an 8 mm-wide slot for the optic nerve. (C) This diagram shows how the plaque can be placed to incorporate the optic nerve and extend beyond the posterior margin of a minimally circumpapillary intraocular tumour. This image was created using the Plaque Simulator Software Program (Bebig, Berlin, Germany).

**Figure 2** Calculation of slot depth.
edges, slotted plaques were gently placed to straddle the retrobulbar optic nerve. Intraoperative three-dimensional ultrasonography was used to confirm plaque placement (fig 3).  

**Case selection**

This study conformed to the Declaration of Helsinki and the United States Health Insurance Portability and Privacy Act of 1996. In this series, the relative risks and potential benefits of observation, radiation (eg, plaque, proton) and enucleation were discussed. Each patient was informed about the number of patients previously treated and chose slotted radioactive plaque therapy.

Case selection and informed consent brought focus on the choice between the potential for vision versus local tumour control. It seemed reasonable to assume that posterior migration of the plaque’s targeted zone (around the optic disc) would increase the incidence of radiation optic neuropathy and the risk of vision loss. However, external beam techniques include more of the optic nerve. When compared with enucleation, all radiation therapy techniques offer some potential for vision retention. Our initial case selection included only those tumours that were not treatable with notched radioactive plaques.

**RESULTS**

Slotted plaques were constructed and used to deliver brachytherapy for the treatment of three patients with intraocular tumours. These included two choroidal melanomas that completely encircled (circumpapillary) and one that was in contact with >180° (juxtapapillary) of the optic disc.

**Illustrative case**

A 33-year-old woman presented with a choroidal melanoma that had encircled (circumpapillary) and displaced the optic disc (fig 4). An 18 mm gold plaque was carved to create an 8 mm-wide and 8 mm-deep slot at its posterior margin. Slot creation eliminated a portion of the posterior sidewall (fig 1). Radioactive seeds were individually placed and affixed (with acrylic) within the plaque, including at positions adjacent to the slot. Once surgically placed, the plaque encircled the optic nerve and covered the entire circumpapillary melanoma and a posterior tumour-free margin. Intraoperative three-dimensional ultrasound imaging confirmed proper plaque placement (fig 3). Preoperative radiation dosimetry confirmed that the tumour received in excess of the minimum tumour dose of 85 Gy.

This patient has been followed up for 16 months. To date, there has been no evidence of tumour growth or complications necessitating secondary treatment. She has lost two lines of visual acuity, with a best corrected Early Treatment Diabetic Retinopathy Study vision of 20/32. Tumour regression has been documented with fundus photography, angiography and ultrasonography. The choroidal melanoma decreased in size and blood flow, with ultrasonographic documentation of tumour regression from 5.2 to 3.1 mm in apical height (fig 3).

Since this case, two additional patients have been treated with slotted-plaque radiation therapy. To date, no surgical or unusual radiation side effects could be attributed to the use of slotted plaques in these cases. Each tumour has responded to irradiation. Follow-up has been <1 year in each of these additional cases.

**DISCUSSION**

Slotted-plaque radiation therapy is ideally suited for current low-energy (21–28 keV) plaque techniques using $^{125}$I and $^{103}$Pd. This is because the radioactive components of these plaques are rice grain-sized seeds whose strength and location can be modulated, conforming to the location and size of the tumour, plaque and slot. In contrast with slotted $^{125}$I and $^{103}$Pd eye plaques, Ru$^{106}$ plaques are not designed to irradiate within the minimum 8 mm-wide slot. While such a configuration might be possible, the manufacturer should only shape Ru$^{106}$ eye plaques. Cutting into a Ru$^{106}$ plaque would create a serious radiation-safety hazard.

In comparison to external beams (eg, radiosurgery, the γ knife and proton beam), slotted-plaque therapy offers the most conformal tumour treatment (much less irradiation of normal anterior ocular and adnexal structures). For example, after stereotactic radiosurgery for juxta papillary melanomas, Simpson et al reported short-term (18-month) actuarial rates of secondary neovascular glaucoma, cataract, retinopathy and optic neuropathy of 20%, 29%, 30% and 37%, respectively. When compared with external-beam radiation therapy techniques, slotted-plaque therapy will deliver less radiation to both the anterior segment and the optic nerve (posterior to the plaque).

This study demonstrates that slotted radioactive plaques can be used to create a “target” zone that includes the entire optic nerve head and adjacent intraocular tumour. This design improves our ability to match tumour and plaque location. In

![Figure 3](http://bjophthalmol.com)

**Figure 3** Finger’s slotted-plaque radiation therapy. A series of intraoperative three-dimensional B-scan ultrasound (3DUS) reconstructions of patient 1. (A) The hyper-reflective eye plaque, delineated by the measurement cursor is seen to cover the longitudinal section of the tumour. (B) A two-dimensional coronal C-scan reconstruction reveals the plaque in position, incorporating the echolucent optic nerve. (C) 3DUS reconstruction allows simultaneous C-scan coronal imaging of the plaque-optic nerve interface as well as the plaque centration over the tumour.
REFERENCES


Figure 4  Finger’s slotted-plaque radiation therapy. (A) Composite photographs demonstrating the pretreatment juxtapapillary melanoma and its early-phase fluorescein angiographic appearance. (B) Note the double circulation seen within its mushroom extension. (C) Sixteen months after slotted-plaque radiation therapy, the tumour is smaller, the mushroom extension is darkened and shrunked, and the optic nerve is less tilted. There is considerable chorioretinal atrophy along its anterior margin. (D) Corresponding fluorescein angiography reveals decreased tumour circulation, optic disc leakage and cystoid macular oedema.

this series, radiation dosimetry studies demonstrated that juxtapapillary and circumpapillary choroidal melanoma received at least the minimum (apical) tumour dose. Thus, Finger’s slotted plaques could be considered as an alternative to external beam irradiation as well as an eye and vision-sparing alternative to enucleation for selected intraocular tumours that touch or surround the optic disc.

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Corresponding interests: None declared.

PTF has a United States Patent pending for a “Slotted Plaque Therapy Device”.

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