Flicker observation light induces diameter response in retinal arterioles: a clinical methodological study

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Aim: To investigate diameter changes in retinal arterioles in response to flicker variations of the examination light.

Methods: One randomised eye of five healthy subjects (mean age 33.8 (SD 1.6) years) was examined. The arterial diameter response to flicker light (12.5 Hz, 530–600 nm, duration 20 seconds) was automatically and continuously measured online three times by retinal vessel analyser (RVA) and once offline from flash images using the VesselMap program.

Results: An arterial diameter response to flicker light was found both by RVA and by analysis of flash images (p<0.001). The maximum induced dilation reached at the end of the flicker period was 7.4% (SD 2.4%) in the RVA measurements and +3.5% (0.8%) in the photographs (p=0.01). In both techniques the vascular diameter overshot the baseline approximately 10 seconds. In the RVA measurements a minimum of −4.6% (1.9%) (p=0.01) was measured 22 (4.7) seconds after the end of flicker exposure.

Conclusion: Flicker evoked response for retinal arterioles was found both by RVA and by analysis of flash images. The authors believe that the method is suitable for the quantitative investigation of retinal vasosclerosis, especially in association with arteriosclerotic and hypertensive systemic disease.

Materials and Methods

One eye of five healthy volunteers (mean age 33.8 (SD 1.6) years, refractive error <1 dioptre) was examined. At the start of the study the ophthalmological baseline status was determined and mydriasis was induced with tropicamide. The fundus was examined under green light. After a period of at least 1 minute, during which the eye was allowed to adapt to the retinal camera, online measurements with the RVA were commenced. After the baseline vessel diameter was measured for at least 60 seconds, provocation with flicker light of the same wavelength was performed for 20 seconds, and the response was observed for at least 60 seconds after the end of flicker exposure. The cycle was then repeated twice. Using the same position, filter, and focus setting on the retinal camera the flicker provocation of 20 seconds was repeated and the vessel response observed by flashed images. During the examination, the systemic blood pressure (BP) was monitored at 1 minute intervals.

The vessel diameter was measured with the RVA (Imedos Weimar, Germany). This consists of a retinal camera, a CCD measuring camera for electronic online image acquisition, and a PC for system control, analysis, and archiving of the results. An artificial vessel section of each eye measuring approximately 1.5 mm in length was evaluated. The vessel section was scanned in the measurement window at a frequency of 25 per second. The positions of the vessel edges were determined and the angle and diameter of the vessel were calculated automatically online. In the process, corrections were made for eye movements along the direction of measurement. The means of all segments of the vessel section in the measurement window were analysed. For statistical purposes, the means for 5 second time intervals were calculated.

The fundus images were taken with the RVA using the FF 450 retinal camera (Zeiss, Jena, Germany) and the VisualIS electronic image processing and archiving system (Imedos, Weimar, Germany). The vessel diameter was automatically determined on the digitised black and white images using the VesselMap program (Imedos, Weimar, Germany). Following correction for the image position, an analysis window was placed over the vessel segment, and the diameter was then measured online three times by retinal vessel analyser (RVA) and once offline from flash images using the VesselMap program.
measured fully automatically in a procedure similar to that used with the RVA. Again, the mean of the vessel segment was used and, for statistical analysis, the measurements of images of 5 seconds long time slices were combined. Flicker light was generated by means of rectangular interruption of the green observation light of the RVA (530–600 nm, illumination at the fundus approximately 6500 lux) at 12.5 Hz over the entire 30° image field.

Variance analysis for repeated measurements and the Wilcoxon test were applied to the data for statistical evaluation.

The study was approved by the ethics committee of the Thuringia State Medical Board, and all the subjects gave their written informed consent to participate in the study.

RESULTS
A diameter response of retinal arteries caused by flicker light could be observed by both examinations methods (ANOVA, in each case p < 0.001, figs 1 and 2). The peak diameter response immediately after flicker provocation was +7.4% (SD 2.4%) in the RVA measurements and +3.5% (0.8%) in the flash photograph analysis (in both cases p = 0.01). Dilation subsided immediately after flicker exposure, and the vessel diameter overshot the baseline about 10 seconds afterward, resulting in slight constriction. The RVA measurement showed a minimum diameter of −4.6% (SD 1.9%) (p = 0.01) 22 (4.7) seconds after the end of flicker provocation. The systemic blood pressure did not change significantly during the examination.

DISCUSSION
The present study measured the change in the diameter of retinal arteries during and after stimulation by flicker modification of the observation light of the retinal camera and RVA. This involved minor manipulation of the illumination system, whereby the observation light is interrupted. This produces a luminance flicker in the green wavelength range at a frequency of 12.5 Hz, which lies in the optimum luminance flicker range of 10–20 Hz determined by Riva et al.11 The diameter changes we observed with the RVA were greater than those observed in the study by Polak et al.10 One explanation for this could lie in the avoidance of continuous fundus illumination by the new stimulation method and the resulting greater flicker contrast. The temporal course of the arterial response essentially coincided with the RVA observations under mixed flicker light, although our 20 second provocation period was much shorter. We also found that the response subsided rapidly, after which the diameter overshot the baseline value to reach a minimum and then a return to more or less the baseline value, reflecting regulatory overcompensation.

Two different examination techniques, online analysis using a high sampling rate (25 Hz) and offline analysis of individual flash images, showed very similar temporal courses of the response but different peak values. The smaller dilation in the flash image series could be due to the greater light exposure produced by the photographic flash in comparison with the RVA observation light. On the images the flicker acts upon a higher baseline value and in relative terms represents a smaller additional stimulus. Another reason for the smaller response amplitudes in the individual images could be the coarser time resolution of the images, so that the peak response is not always recorded. The images were not taken corresponding to pulse in our study. The heart cycle influences the retinal vessel diameter and therefore the results could be influenced by the random photographic moment. However, the results coincide well with the values determined after flicker light provocation in fundus photograph.17 In view of the lesser stress caused by the method, the greater relative diameter change it induces, and the simpler repetition of the provocation it affords with the possibility of averaging, the RVA technique therefore appears to be the more favourable of the two methods. Further clinical studies are needed now to systematically investigate the influence of age, systemic blood pressure, and anti-hypertensive therapy on the flicker response of retinal arterioles.

Figure 1 Mean arterial response to flicker light measured by RVA (n = 5).

Figure 2 Mean arterial response to flicker light measured in flashed images (n = 5).

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