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The Argus II epiretinal prosthesis system allows letter and word reading and long-term function in patients with profound vision loss

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ABSTRACT

Background Retinal prosthesis systems (RPS) are a novel treatment for profound vision loss in outer retinal dystrophies. Ideal prostheses would offer stable, long-term retinal stimulation and reproducible spatial resolution in a portable form appropriate for daily life.

Methods We report a prospective, internally controlled, multicentre trial of the Argus II system. Twenty-eight subjects with light perception vision received a retinal implant. Controlled, closed-group, forced-choice letter identification, and, open-choice two-, three- and four-letter word identification tests were carried out.

Results The mean±SD percentage correct letter identification for 21 subjects tested were: letters L, T, E, J, F, H, I, U, 72.3±24.6% system on and 17.7±12.9% system off; letters A, Z, Q, V, N, W, O, C, D, M, 55.0±27.4% system on and 11.8±10.7% system off, and letters K, R, G, X, B, Y, S, P, 51.7±28.9% system on and 15.3±7.4% system off. ($p<0.001$ for all groups). A subgroup of six subjects was able to consistently read letters of reduced size, the smallest measuring 0.9 cm (1.7°) at 30 cm, and four subjects correctly identify unrehearsed two-, three- and four-letter words. Average implant duration was 19.9 months.

Conclusions Multiple blind subjects fitted with the Argus II system consistently identified letters and words using the device, indicating reproducible spatial resolution. This, in combination with stable, long-term function, represents significant progress in the evolution of artificial sight.

Retinal prosthesis systems (RPS) are a new treatment for profound vision loss in retinitis pigmentosa.^{1 2} Ideal RPSs would provide stable, long-term retinal stimulation inducing visual percepts that allow form recognition while being safe, practical and portable, so it can be used in the setting of the subject's daily life.^{3 4} Many of these features have been demonstrated in small studies, in differing combinations to date.^{5–13}

Outcome measures of RPSs in blind subjects are being sought, with grating visual acuity, motion detection, tests of orientation and mobility, tasks of daily living, as well as quality-of-life outcomes being investigated.^{14–18} We have chosen letter identification as an outcome measure for spatial resolution in this study as it is currently the most familiar method in conventional clinical trials.^{19–21} However, standard Early Treatment Diabetic

Retinopathy Study (ETDRS) tests are not validated or appropriate for prosthetic retinal devices, and as such, we have used a specific methodology that allows the identification of letters to be assessed using such devices.

The Argus II retinal prosthesis system (Second Sight Medical Products, Sylmar, California, USA) is fully portable and consists of a video camera mounted on glasses, a video processing unit (VPU) and a 60-electrode, epiretinal stimulating array.^{10 13} The array stimulates residual inner retina directly, mainly ganglion and possibly bipolar cells,^{22–24} with the signal transmitted via the normal visual pathway to the visual cortex. The aim of the tests reported here was to determine whether a group of patients blinded by outer retinal dystrophies and fitted with the Argus II system, could identify letters and words on a computer screen as a demonstration of effective spatial resolution, in the context of a device that is stable, portable and capable of long-term function.

METHODS

The Argus II feasibility study is a prospective, multicentre, internally controlled trial registered at (<http://clinicaltrials.gov/show/NCT00407602>). The institutional review boards or ethics committees, and competent authorities of participating sites and countries, approved the protocol. The trial adhered to the tenets of the Declaration of Helsinki.

Subjects/device

Twenty-nine subjects with retinitis pigmentosa, and one with choroideremia with vision reduced to light perception or worse, defined as unable to see gratings of 2.9 logMAR (20/16 000)^{20 21} in either eye, were enrolled in the trial. Two patients are not reported as one had the device explanted due to conjunctival erosion, the other had a retinal detachment. The remaining 28 subjects had functioning electrodes and reportable visual phosphenes at the end of this study, and were documented for long-term function. Twenty-one subjects took part in the letter-reading study. The nine subjects not included are one with silicone oil in situ due to hypotony, one awaiting replacement of their retinal tack, two who declined to participate due to the length of time taken to identify letters during training, three who were excluded due to inconsistencies in executing the test protocol and the two described above. For

each subject, age at diagnosis, age at implantation and the number of months the device had been implanted by the end of the study were recorded. The device consisting of video camera glasses, a VPU and a wireless-activated 60-electrode stimulating array has been described previously.^{10 13}

Letters, monitor and lighting

Letters and words were white on a black background on an external LCD screen with resolution set to 1024×768 pixels (MatLab, Mathworks, Natick, Massachusetts, USA). Optotypes in True Type Century Gothic (CG) font were created in PowerPoint (Microsoft, Redmond, Washington, USA) and viewed at 30 cm. In Test I, the letter size was 41.27°. In Test II, the size was reduced from 41.27° in 0.1 log unit steps to 0.95°. In Test III, the sizes were 33.39° for the two-letter words, 26.81° for the three-letters words and 21.33° for the four-letter words. Testing was carried out in a darkened room.

Training for each test

Standardised training for Test I consisted of showing each subject each of the letters once with the RPS device on and telling them the name of the letter displayed while the patient scanned the screen. There was no further practice carried out before the formal testing. There was no training for Test II, the letter size reduction, or Test III, the word reading.

Test I: letter identification

All subjects were asked to identify all 26 letters. Letters were separated into three groups with differing typographical complexity. Group A only horizontal and vertical components (eg H, I) Group B oblique components involving the full height of the letter (eg, A M W), or letter with a minor variation on a circle (eg, O D C), and Group C letters with an oblique or curved element involving half the letter height (eg, K R) These were presented in a forced-choice, closed-set test in the order A then B then C. Researchers presented letters in random order, one at a time, four times each, both with the system on and off. Subjects who found the earlier groups difficult declined to continue the study for the later groups of letters. Twenty-one subjects completed Group A letters L, T, E, J, F, H, I, U; nineteen Group B letters A, Z, Q, V, N, W, O, C, D, M, and twenty Group C letters K, R, G, X, B, Y, S, P. The time taken to identify each letter was recorded.

Test II: letter size reduction

A subset of six subjects who in Test I correctly identified 50% or more of the letters in each group within 60 s, also completed Test II. Researchers asked subjects to identify the letters C, D, H, K, N, O, R, S, V, Z in a forced-choice, closed-set test; subjects were allowed to guess. Letters were presented individually, in random order, with five letters of each size constituting a 'line', and reducing size in 0.1 log unit steps. A time limit of 60 s per letter was set. The stopping point was five errors in any line, or when the subject felt that they were unable to guess the letter. Researchers carried out test and control runs twice, on separate days.

The total number of letters correctly identified, and height of the smallest correct letter (minimal letter size (MLS)) were recorded. The equivalent number of correct lines was calculated by dividing the number of correct letters by 5. The letter size of the smallest line using this calculation was recorded as the optimal letter size (OLS).

Test III: word recognition

Four subjects who scored more than 10 letters correct in Test II completed Test III. Common two-, three- and four-letter words in English or French, from word frequency tables, were presented in the subject's preferred language. Letter spacing was standard for the font size with no additional spacing created between the letters. A time limit of 120, 180 and 240 s for two-, three- and four-letter words was set with a warning 10 s before the end.

Test and control conditions

For Test II letters and Test III words, the five tested conditions were: system off and both eyes unpatched; system on in 'scrambled' mode with eyes patched and unpatched; and system in standard mode with eyes patched and unpatched. The scrambled mode²⁵ consisted of the system being on but the spatial mapping of the image onto the electrodes randomised so the spatial correlation between camera image and retinal stimulation was lost (figure 1D).

Statistical analysis

Researchers used the Wilcoxon signed rank test to examine the significance of the difference between conditions for each of the groups tested, and standard multiple regression to determine how much variance in the percentage of correct letter identification could be explained by three independent variables: age at implantation, age at diagnosis and number of electrodes activated. For Test II, a statistical analysis was done by first using a one-way analysis of variance (ANOVA) model to determine whether the number of correct answers was significantly influenced by the system condition. Second, another one-way ANOVA analysis was performed to determine whether the number of correct answers (with the system ON and standard mode) was significantly influenced by the different patching conditions.

RESULTS

Subjects and implant

Gender, age at diagnosis and at implantation, duration of implantation and number of electrodes included in the video configuration file at the time these tests were conducted are recorded in table 1. Average implantation duration was 19.9 months (range 8.6–34.8) at test completion, with all devices demonstrating functioning electrodes throughout testing.

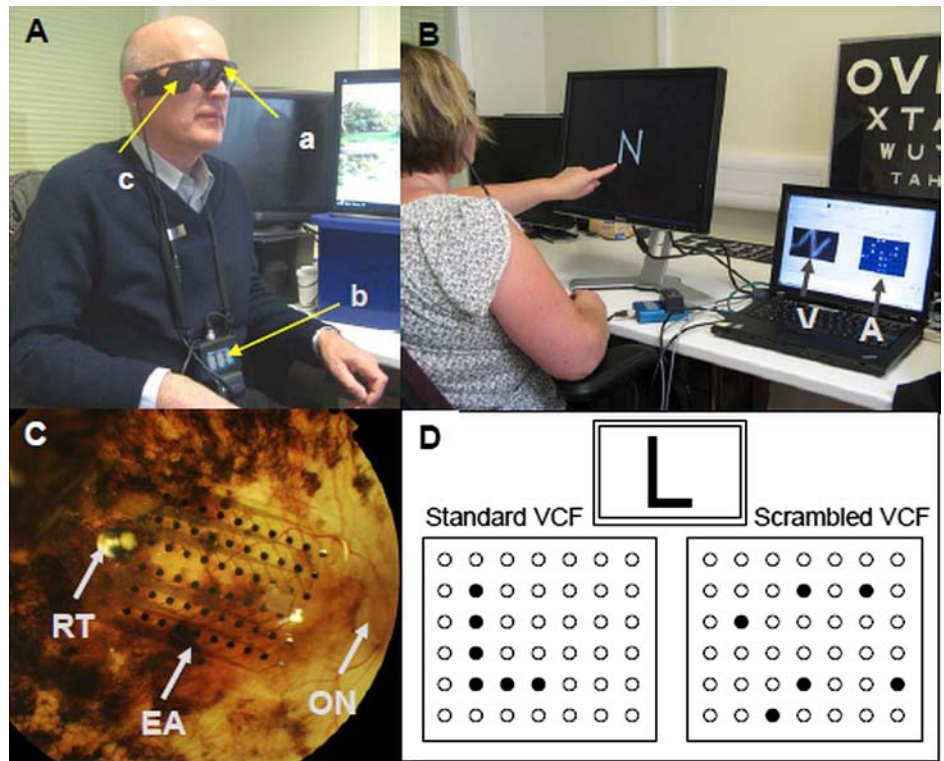
Test I

Mean percentage correct±SD for subjects tested were: Group A 72.3±24.6% system on and 17.7±12.9% system off; Group B 55.0±27.4% system on and 11.8%±10.7% system off and Group C 51.7%±28.9% system on and 15.3%±7.4% system off. ($p<0.001$, device on versus off for all groups—Wilcoxon signed ranks test). The median and quartile ranges for outcomes are shown in figure 2. The average times (in seconds) for correctly identified letters (system on) were 47.7, 68.6 and 63.9 for Groups A, B and C, respectively.

Test II

The MLS and OLS in cm (degrees) viewed at 30 cm for subject 51-009 are 0.9 (1.7°) and 5.6 (10.6°); 52-001, 1.8 (3.4°) and 3.6 (6.8°); 61-005, 1.1 (2.1°) and 2.3 (4.3°); 61-003, 3.6 (6.8°) and 14.3 (27.1°); 12-005, 3.6 (6.8°) and 14.3 (27.1°); and 52-003, 18.0 (32.4°) and 22.6 (42.9°). The average number of

Figure 1 (A) Photograph of a subject with the Argus II system showing the video glasses (a), the Video processing unit (b) and the inductive coil (c). (B) Subject showing the format for the letter identification tasks with a letter displayed on a monitor in white on black, Century Gothic font. The monitor on the side shows the real time map of the electrodes being stimulated in the array (A) and the camera view (V); note that the actual test is carried out in the dark. (C) Fundus photograph of the retinal stimulating array in situ. The optic nerve is indicated and the retinal tack that secures the electrode array is clearly visible. (D) Diagram illustrating the difference between the electrode activation maps under the 'home use' (standard) and 'scrambled' mode when the camera is viewing the letter L. In the scrambled mode, the spatial correspondence between a point's real position and the stimulation position on the array has been randomised. In this way, the patient does not receive spatial information but does receive non-spatial light detection information.



letters correctly identified for each test modality is summarised in figure 3.

Test III

The tabulated results of the number correct in word recognition for two-, three- and four-letter words for each of the test situations is reported in table 2. The results show there is a clear improvement for all four subjects with the device on (both patched and unpatched).

Multiple regressions (Test I)

After adjusting for the small sample size, the three variables, age at implantation, age at diagnosis, and number of electrodes activated jointly, explained 19% (ns), 27% (ns) and 39% ($p < 0.01$) of the variances for correct letter identification in Test I, Groups A, B and C letters, respectively. For all three groups of letters, number of electrodes and age at the time of implantation made the largest unique contributions to the percentages above. Only age at implantation correlated singly with statistical significance and explained 30% (ns), 36% ($p < 0.01$) and 28% ($p < 0.01$) of the total variances for Groups A, B and C letters, respectively.

DISCUSSION

The research team have investigated the Argus II system both in terms of spatial resolution, using letter identification, and long-term stable function. In Test I on average, across all the subjects, letters could be clearly identified correctly between 51.7% (Group C) and 72.3% (Group A) of the time with the system on while performing at chance level with the device off. The median values for correct letters, system on, in figure 2 of 50% or greater for groups A, B and C indicate that at least half the group was functioning at this level (figure 2).

It is possible that a component of letter identification involves head scanning with light detection and inference of the letter. This may partially account for the greater number correct for

Group A letters when the Test I letters were stratified into three groups of increasing typographic complexity. However, experimenters observed that many high-performing subjects did not scan across the letter but followed the form of the letter as if tracing it, suggesting that they were able to see the straight and curved strokes that make the form of the letter. Furthermore, failure to identify letters in Test II with the scrambled mode (not better than device off) showed that letter identification is not primarily dependent on head scanning, light detection and inference, but uses the spatial information contained in the percept. The two outlier patients (figure 2 device off) may have used residual light perception to construct a sense of the letter to aid guessing in the less complex letters in Groups A and B. However, in both subjects, the letter-reading performance was both better and faster with the device on.

Test II examined six high-functioning subjects in terms of the limit of letter size identification. The study team used the framework of the ETDRS letter set and layout, with five letters per 'line' and 0.1 log unit steps. CG font was chosen to maximise the chance of recognition with an RPS as the narrow lines of the font maximised the space between linear elements and presented a low mean illumination. Unlike the standard ETDRS test, the letters were presented one at a time in white on a black background.

The best subjects were able to consistently identify letters from 2.3 cm, (4.3°) to 22.6 cm, (42.9°) in height (OLS). The smallest letters identified ranged from 0.9 cm (1.7°) to 18 cm (34.2°). As the electrode spacing in the array is 1.8° , this shows that, in at least some subjects, the system is working at a level approximating predicted limit of spatial resolution. This was also shown previously for the Argus I device.²⁵ As expected, there were significant errors at the smaller sizes. The scrambled mode control confirmed that letter recognition was based on true spatial resolution and not light detection. Patching confirmed that the outcomes were not achieved due to residual

Table 1 Data relating to subjects implanted with the Argus II

Subject	Sex	Age at diagnosis (years)	Age at surgery (years)	Months implanted	Electrodes activated
11-001	F	23	55	34.8	37
11-002	F	54	61	34.5	*
12-001	M	30	52	†	
12-002	F	32	60	34.6	53
12-003	M	42	75	34.6	40
12-004	M	26	52	34.2	14
12-005	M	43	70	10.0	54
13-001	M	9	49	10.1	5
13-002	F	37	52	9.5	*
14-001	F	13	56	10.2	20
15-001	M	25	58	31.6	18
15-003	F	24	77	24.9	21
17-001	F	35	55	‡	
17-002	M	22	66	33.7	30
51-001	M	20	70	24.5	26
51-002	M	16	51	24.5	*
51-003	M	19	72	22.9	28
51-005	M	7	55	13.2	60
51-006	M	46	66	12.2	*
51-007	M	28	63	10.5	56
51-009	F	11	45	8.6	60
52-001	M	30	50	10.9	60
52-002	M	16	65	11.3	29
52-003	M	25	60	8.8	37
61-001	M	3	53	26.6	11
61-003	M	34	57	15.3	51
61-004	M	20	59	13.2	6
61-005	M	12	49	11.1	40
71-002	M	15	60	26.6	29
71-003	F	2	28	13.9	36

M, male; F, female; Age at diagnosis, age at the diagnosis of the outer retinal dystrophy; Age at surgery, age at implantation of the Argus II system; Months implanted, the number of months from implantation to the end of this study; Electrodes activated, the number of electrodes in use during this testing.

*Did not take part in letter reading tasks.

†Retinal detachment.

‡Explanted: conjunctival erosion/exposure.

native light perception or a placebo effect. We feel that the OLS gives a better functional indication of the size where letter identification was consistent. We used letter height as the outcome, as CG letters do not have the equivalent defining elements within each character as Sloan letters in the ETDRS set. As such, the outcome is a descriptive indication of the functional level of letter identification possible rather than a formal visual acuity measure.

Four subjects from the same high-performing group could also read short words. This demonstrated the ability to define separate letters with minimal spacing and not to confuse multiple letters. Due to the small sample size, a statistical analysis was not performed. Nevertheless, these results support the proof of principle that this device allows simple word reading. True spatial resolution was indicated, as there was no consistent word reading with the scrambled control. Letter reading has been previously reported in a patient with a subretinal implant with resolution 'corresponding to a height of approximately 9° of visual angle'. The subject was described as being able to identify 16 different cut-out letters, and read five words correctly 'repeatedly on several days'.¹² A few words were correctly

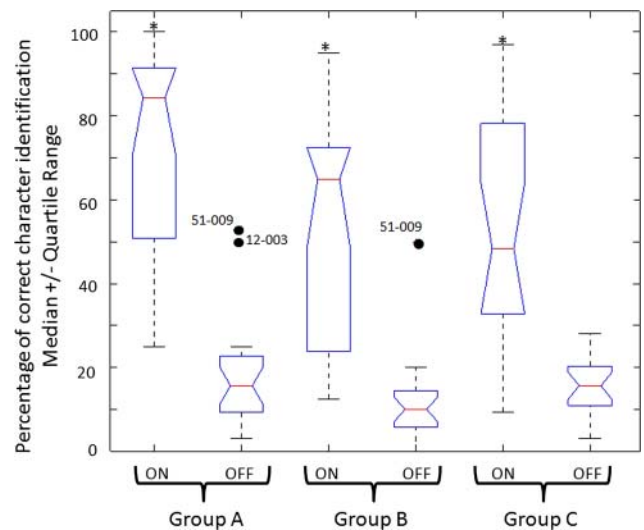


Figure 2 Box and whisker graphs illustrating the median percentage correct and quartiles for Test I letter Groups A, B and C comparing the device on and off. For Groups A, B and C, n=21, 19 and 20, respectively. (** <math><0.001</math> Wilcoxon signed rank test). Outliers, shown as black dots, are data with values beyond the ends of the whiskers.

identified when viewed with eyes unpatched and the device off or in scrambled mode. We feel that the residual light perception, with or without the Argus II acting as a light detector, may have led to a sense of the letter or word allowing enhanced guessing. With the device in scrambled mode and both eyes patched, the two correct identifications were likely lucky guesses.

Despite the good overall level of letter identification, the average time taken to correctly identify letters in Test I ranged across subjects from 6 s to 221 s. What differentiates high-functioning subjects from others is not clear at present. Multiple regression analysis suggests that age at implantation correlated to letter reading outcome with statistical significance. This may reflect the presence of healthier residual inner retina. Age at diagnosis and number of electrodes activated (see table 1) also correlated to better outcome with letter identification, though not statistically significantly, likely reflecting the small sample size. Genotype may play a part, but the number of cases in this study with a known genotype precludes investigation of this issue. Identifying these factors will be important in informing

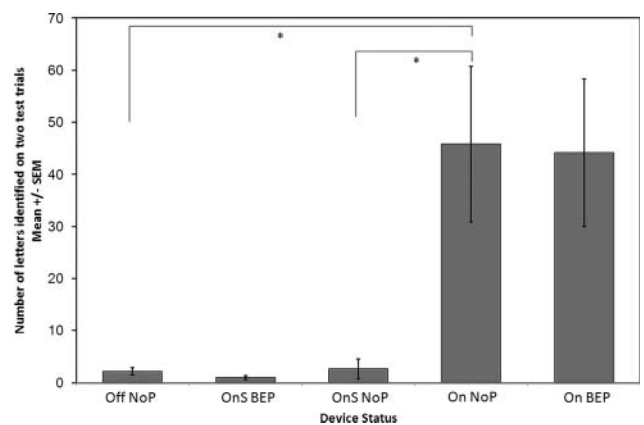


Figure 3 A graph showing the mean and SEs of the total number of letters identified correctly in two test runs of letter size reduction using the Argus II retinal prosthesis system. (*

Table 2 Word reading outcome table

Subject	System off Unpatched	System on scrambled mode		System on standard mode	
		Unpatched	Patched	Unpatched	Patched
Two-letter words (10 words per trial)					
51-009	2	1	0	8	8
52-001	1	0	1	10	7
61-003	0	0	0	7	7
61-005	0	0	0	5	10
Three-letter words (10 words per trial)					
51-009	1	0	0	6	7
52-001	1	2	0	6	6
61-003	0	0	0	5	5
61-005	0	0	0	8	9
Four-letter words (10 words per trial)					
51-009	0	0	1	5	7
52-001	1	1	0	5	6
61-003	0	0	0	3	4
61-005	0	0	0	10	9

Table summarising the number (out of 10) of two-, three- and four-letter words read correctly by the four subjects in five conditions. The test conditions are indicated by the column labels.

future case selection. Also, it is not immediately clear how the performance of the controlled tasks identified in this study will translate directly into useful function in daily life, and this is being studied further.

The Argus II RPS was stably fitted into the 28 subjects for an average time of 19.9 months (range 8.6–34.8) from implantation to the end of the tests in this study. Throughout the study, 28 out of 30 implants had functioning electrodes (as recorded in table 1), thus demonstrating the possibility for stable chronic stimulation. Of the other retinal prosthesis trials, the Optobionics chip was reported stable in the eye for up to 18 months,⁹ the Argus I to more than 5 years²⁵ and the subretinal implant study up to 5 weeks.⁷

CONCLUSION

This study demonstrates that the Argus II RPS shows features required of a successful artificial retina system. In accordance with this, it became the first retinal prosthesis to receive regulatory approval for implantation in Europe outside of a trial, in April 2011. This paper highlights a large number of subjects that are able to identify letters, and a group identifying words successfully. The device is portable; remains functional currently for up to 34 months, and has been implanted successfully in multiple centres worldwide. This study adds to the growing evidence that retinal prosthetic devices will play a role in the treatment of profound vision loss in outer retinal dystrophies in the future.

Contributors LdC, GD, BFC, JD, FM, EF, PC and VW made substantial contributions to conception and design, acquisition of data, and analysis and interpretation of data; JS, PS, FKC, MH, RJG made substantial contributions to acquisition of data, and analysis and interpretation of data. All authors, in addition, were involved in drafting the article and revising it critically for important intellectual content and final approval of the version to be published.

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Competing interests LdC, EF, FKC, JS, PS and GD have no financial interests. BFC, JD, FM, PC, VW are employees of Second Sight Medical Products Inc, but have

no financial interest. MH and RJG have a financial interest in the Argus II retinal prosthesis system.

Ethics approval Commission centrale d'éthique de la recherche sur l'être humain, Geneva/East London Research Ethics Committee, Bristol/Comité de protection des personnes—Ile de France V, Paris.

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REFERENCES

- Zrenner E. Will retinal implants restore vision? *Science* 2002;295:1022–5.
- Rizzo JF, O'Malley ER, Hessburg PC. The eye and the chip 2008. *J Neural Eng* 2009;3:030201.
- Weiland JD, Liu W, Humayun MS. Retinal prosthesis. *Annu Rev Biomed Eng* 2005;7:361–401.
- Zrenner E. The subretinal implant: can microphotodiode arrays replace degenerated retinal photoreceptors to restore vision? *Ophthalmologica* 2002;216(Suppl 1):8–20.
- Rizzo JF III, Wyatt J, Loewenstein J, et al. Perceptual efficacy of electrical stimulation of human retina with a microelectrode array during short-term surgical trials. *Invest Ophthalmol Vis Sci* 2003;44:5362–9.
- Yanai D, Weiland JD, Mahadevappa M, et al. Visual performance using a retinal prosthesis in three subjects with retinitis pigmentosa. *Am J Ophthalmol* 2007;143:820–7.
- Besch D, Sachs H, Szurman P, et al. Extraocular surgery for implantation of an active subretinal visual prosthesis with external connections: feasibility and outcome in seven patients. *Br J Ophthalmol* 2008;92:1361–8.
- Rössler G, Laube T, Brockmann C, et al. Implantation and explantation of a wireless epiretinal retina implant device: observations during the EPIRET3 prospective clinical trial. *Invest Ophthalmol Vis Sci* 2009;50:3003–8.
- Chow AY, Chow VY, Packo KH, et al. The artificial silicon retina microchip for the treatment of vision loss from retinitis pigmentosa. *Arch Ophthalmol* 2004;122:460–9.
- Humayun MS, Dorn JD, Ahuja AK, et al. Preliminary 6 month results from the argus II epiretinal prosthesis feasibility study. *Conf Proc IEEE Eng Med Biol Soc* 2009;1:4566–8.
- Horsager A, Greenberg RJ, Fine I. Spatiotemporal interactions in retinal prosthesis subjects invest. *Ophthalmol Vis Sci* 2010;51:1223–33.
- Zrenner E, Bartz-Schmidt KU, Benav H, et al. Subretinal electronic chips allow blind patients to read letters and combine them to words. *Proc R Soc B* 2011;278:1489–97.
- Ahuja AK, Dorn JD, Caspi A, et al. Argus II study group blind subjects implanted with the Argus II retinal prosthesis are able to improve performance in a spatial-motor task. *Br J Ophthalmol* 2011;95:539–43.
- Chader GJ, Weiland J, Humayun MS. Artificial vision: needs, functioning, and testing of a retinal electronic prosthesis. *Prog Brain Res* 2009;175:317–32.
- Dagnelie G. Psychophysical evaluation for visual prosthesis. *Annu Rev Biomed Eng* 2008;10:339–68.
- Geruschat DR, Turano KA, Stahl JW. Traditional measures of mobility performance and retinitis pigmentosa. *Optom Vis Sci* 1998;75:525–37.
- Szyk JP, Fishman GA, Alexander KR. Relationship between difficulty in performing daily activities and clinical measures of visual function in patients with retinitis pigmentosa. *Arch Ophthalmol* 1997;115:53–9.
- Massof RW. The measurement of vision disability. *Optom Vis Sci* 2002;79:516–52.
- Kaiser PK. Prospective evaluation of visual acuity assessment: a comparison of snellen versus ETDRS charts in clinical practice (an AOS thesis). *Trans Am Ophthalmol Soc* 2009;107:311–24.
- Schulze-Bonsel K, Feltgen N, Burau H, et al. Visual acuities 'hand motion' and 'counting fingers' can be quantified with the Freiburg visual acuity test. *Invest Ophthalmol Vis Sci* 2006;47:1236–40.
- Bach M, Wilke M, Wilhelm B, et al. Basic quantitative assessment of visual performance in patients with very low vision. *Invest Ophthalmol Vis Sci* 2010;51:1255–60.
- Matthaei M, Zeitz O, Kesper M, et al. Progress in the development of vision prostheses. *Ophthalmologica* 2011;225:187–92.
- Humayun MS, Weiland JD, Fujii GY, et al. Visual perception in a blind subject with a chronic microelectronic retinal prosthesis. *Vision Res* 2003;43:2573–81.
- Greenberg RJ, Velte TJ, Humayun MS, et al. A computational model of electrical stimulation of the retinal ganglion cell. *IEEE Trans Biomed Eng* 1999;46:505–14.
- Caspi A, Dorn JD, McClure KH, et al. Feasibility study of a retinal prosthesis: spatial vision with a 16-electrode implant. *Arch Ophthalmol* 2009;127:398–401.